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Characterization of Skin Permittivity for Human Fingers by Open-ended Waveguide at Sub-THz

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Abstract— This paper proposes a method for characterizing the complex permittivity of the human finger skin based on an open-ended waveguide covered with a thin dielectric sheet at sub-terahertz frequencies. The measurement system is initially analyzed through full-wave simulations with a detailed finger model. Next, the model is simplified by replacing the finger with an infinite sheet of human skin to calculate the forward electromagnetic problem related to the permittivity characterization. Following this, a radial basis network is employed to train the inverse problem solver. Finally, the complex permittivities of finger skins are characterized for 10 volunteers. The variations in complex relative permittivity across different individuals and skin regions are analyzed, revealing a deviation of < 2 for both the real and imaginary parts of permittivity across 140 to 220 GHz. Repeated measurements at the same location on the finger demonstrate good repeatability with a relative estimation uncertainty $< \pm 1.4\%$.

Keywords— Human skin permittivity, sub-THz, finger permittivity, radial basis network, forward problem model

I. INTRODUCTION

The sub-terahertz (sub-THz) band has garnered attention from researchers in the telecommunication community due to its potential for high data-rate transfer [1], [2]. Handset antennas are sensitive to the radio environment, especially in close proximity to obstructions such as fingers, hand palms, and human bodies [3]. To investigate human-antenna interaction for enhanced handset antenna designs, knowledge of the permittivity of human tissues becomes crucial. However, there exists a notable scarcity of research addressing sub-THz frequencies, with a lack of measurement-based permittivity estimates for human tissues such as fingers, palms, and the body. The skin depth of typical human skin in millimeter wave (mmW) bands is less than 2 mm, according to the formulas provided in TABLE 1.1 of [4]. Consequently, it is appropriate to model the effects of humans on antennas as a skin-antenna interaction at mmW [5] and sub-THz.

Permittivity measurements have been conducted beyond 60-GHz frequencies in various studies [6]–[9]. Many of these investigations rely on the transmission and reflection of electromagnetic waves, primarily targeting layered materials. As a consequence, these methods are typically applicable only to flat slices of human skin. In practical scenarios, it becomes essential to conduct measurements on living skin to study realistic effects on mobile terminal antennas. To address this need, the open-ended probe method has been employed in 5G mmW bands for characterizing human skin permittivity in [10], [11], where some important parts of

human skin, including fingers, palms and arms, were measured, yielding convincing permittivity estimates for human-antenna interaction studies. In this paper, we extend this open-ended probe method to sub-THz frequencies to measure human finger skin permittivity. Differing from previous publications, we propose a machine-learning approach where a simplified full-wave simulation model is used to train a neural network for estimating human skin permittivities.

II. PERMITTIVITY CHARACTERIZATION

A. Human Skin Characteristics in Sub-THz Bands

Several researchers have proposed a multi-layer human skin model for THz bands [12]–[14]. Utilizing Eq.(4) in [15], typical effective relative permittivities are $2.7 - 0.1i$ for the stratum corneum, $3.3 - 5.2i$ for the epidermis, and $3.9 - 5.2i$ for the dermis at sub-THz frequencies. As indicated by [12], the thickness of the stratum corneum varies from $15 \mu\text{m}$ on arms to $300 \mu\text{m}$ on fingers. Consequently, the effective permittivity of human skin at sub-THz frequencies differs depending on anatomical locations and varies among individuals [12].

B. The Problem of Existing Method

The WR5 (140 – 220 GHz) extender of the vector network analyzer (VNA) is equipped with an open-ended waveguide featuring a flange, enabling the measurement of finger permittivities without the need for designing a new probe. When using the method, the measured reflection coefficients are more sensitive to pressure exerted by fingers on the open-ended waveguide than in 5G mmW-band measurements [10]. Increased pressure results in more parts of the finger being pressed into the open-ended waveguide, introducing a skin protrusion problem that leads to significant inaccuracies in estimating finger permittivities [10]. To mitigate this, [10] used copy papers to flatten the skin's surface and improve measurement accuracy in 5G mmW bands. Although copy papers between the waveguide and finger can reduce skin protrusion compared to the finger without the papers, even a tiny protrusion can cause a significant measurement deviation at sub-THz. Consequently, the effectiveness of this approach is limited at sub-THz, since copy papers are soft and, therefore, easily deformable.

C. Our Proposed Method

To address the mentioned limitations, we employ a hard and thin sheet placed on the open-ended waveguide. Following

the findings in [8], the thickness of the sheet should be smaller than 0.1 wavelength to reduce electromagnetic emissions along the flange plate directions and higher transmission modes of waveguides. Consequently, we opt for a hard sheet, specifically Rogers 4350B, with a relative permittivity $\epsilon_s = 3.33 - 0.0123i$ and a thickness of $W_s = 0.1$ mm. An open-ended waveguide can be an antenna that excites waves along the flange. When the sheet is thin enough, the surface wave along the flange will be easily attenuated by the high-loss human tissues. When the contact area of the firmly pressed finger on the sheet is large enough, we can consider the surface waves to be completely attenuated. To determine the required contact area, full-wave simulations are implemented, as illustrated in Fig. 1. The waveguide flange radius is $R_f = 6$ mm, while the sheet radius is also $R_s = 6$ mm. We assume that finger skin permittivity is $\epsilon_r = 4.0 - \frac{16.0}{\epsilon_0 \omega}i$, following the knowledge presented in [15], where ϵ_0 is the vacuum permittivity, and ω is the angular frequency.

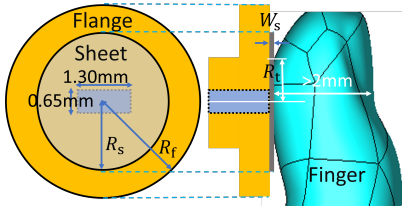


Fig. 1. The front and side views of the simulation model to study the effects of the varying contact area radius. Finger skin permittivity: $\epsilon_r = 4.0 - \frac{16.0}{\epsilon_0 \omega}i$.

We vary the radius of the contact area between the skin under measurement and the sheet (R_t) from 1.0 mm to 3.0 mm, and also consider the case where $R_t = \infty$. The magnitudes of reflection coefficients at the open end of the waveguide are depicted in Fig. 2a. Observing the results, it becomes evident that for $R_t > 2.0$ mm, the reflection coefficients closely resemble those obtained at $R_t = \infty$. Additionally, $R_t \geq 2.0$ mm introduces less than 0.5° difference compared to $R_t = \infty$ in Fig. 2b. To accommodate variations in finger permittivity among different individuals, practical measurements necessitate $R_t > 3.0$ mm. This ensures that external factors like positioning pins or other structures of the open-ended waveguide, which may cause disturbance to waves, do not significantly influence the measured reflection coefficients. This approach allows treating both the sheet and human skin as infinitely large in the context of measurements, and therefore also allows to use a simplified simulation model to produce training data for machine learning.

When we change the human skin permittivities from 3 to 6 for the real part and from 1 to 4 for the imaginary part, which is a probable human skin permittivity range based on the knowledge in [15], $R_t > 3.0$ mm can still offer a high accuracy as $R_t = \infty$. For brevity, the reflection coefficients of these permittivity values are not shown here. However, for other frequency ranges, we may need to change the size of the contact area in measurements. Therefore, we need rough prior knowledge of human skin permittivity.

The forward electromagnetic problem of permittivity

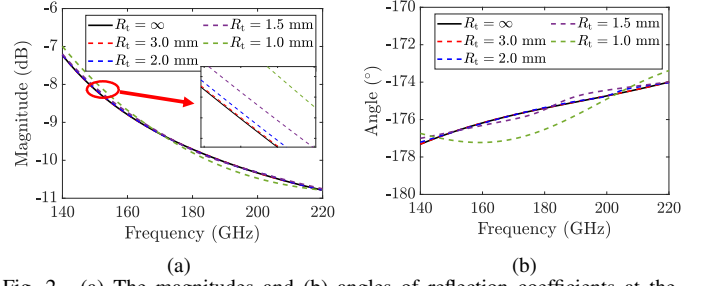


Fig. 2. (a) The magnitudes and (b) angles of reflection coefficients at the open end of the waveguide covered by a finger with different R_t as shown in Fig. 1.

measurements is formulated as $\Gamma = F(\epsilon_r)$, where Γ is the reflection coefficient at the open end of the waveguide, and ϵ_r is the complex permittivity. The simplified simulation model for the forward problem, depicted in Fig. 3, is constructed using *CST Studio Suite* and solved in the frequency domain. In the model, the blue region represents 'air' in the waveguide, and the background material, highlighted in gray, is a perfect electric conductor (PEC). The dimensions of the skin are $6 \times 6 \times 3$ mm³, while the Rogers 4350B sheet measures $6 \times 6 \times 0.1$ mm³. The reference plane for the reflection coefficients is the open end of the WR5 waveguide, consistent with the measurement setup. The boundary of the box enclosing the entire model is set to 'open', ensuring the PEC fills the box. This setup allows the simulation model to emulate an infinite sheet and finger skin, meeting the same conditions as the measurements. To extract the reflection coefficients at the open end of the waveguide, the length of the waveguide is de-embedded. The TE₁₀ mode is excited at the waveguide input.

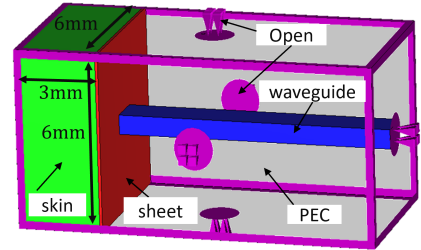


Fig. 3. The calculation model of the forward problem.

To derive the inverse-problem solver, i.e., $\epsilon_r = F^{-1}(\Gamma)$ for permittivity characterizations, we utilize a radial basis network (RBN)¹. The input parameters of the solver consist of Γ_r and Γ_i , representing the real and imaginary parts of the reflection coefficients. The outputs are denoted by ϵ' and ϵ'' , corresponding to the real and imaginary parts of the relative permittivity.

Finger permittivity estimation involves the following steps:

- 1) Calibrate the vector network analyzer (VNA) at the interface of the open-ended waveguide.
- 2) Place a finger on the open end of the waveguide with the Rogers 4350B sheet in between, and record the reflection coefficients Γ across the frequency range.

¹Functions such as 'newrb' in *MATLAB* can be employed for this purpose.

- 3) Repeat step 2) for different parts of fingers from multiple individuals.
- 4) Obtain training data by simulating the setup illustrated in Fig. 3 and then train the inverse-problem solver based on RBN using this data.
- 5) Input the measured Γ values into the trained inverse-problem solver to estimate the finger permittivity at each frequency.

III. FINGER PERMITTIVITY CHARACTERIZATION

A. Training Data

The spread of the radial basis network was set to 1.0. Utilizing prior knowledge about human finger permittivity presented in Section II-A, the training data is generated by sweeping the real part of skin permittivity from 3 to 6 and the imaginary part from 1 to 4 with 25 and 40 uniformly distributed samples, respectively. The total number of samples is 1000. The full-wave simulation frequency varies from 140 GHz to 220 GHz across 1001 uniformly sampled points.

The relative mean error of complex permittivity is defined as $err = \frac{|\epsilon_r - \bar{\epsilon}_r|}{|\epsilon_r|}$, where ϵ_r is the true value, and $\bar{\epsilon}_r$ is the estimate. After simulating reflection coefficients, the dataset is split into 90% training data and 10% testing data. The relative mean error of complex permittivity for testing data is less than 0.05%, indicating high estimation accuracy. It is noteworthy that, to simplify the training model, the inverse problem solver is trained for each frequency point individually, which can lead to more reliable results considering frequency-dependent permittivities.

B. S-parameter Measurements

The measurement setup is illustrated in Fig. 4. During

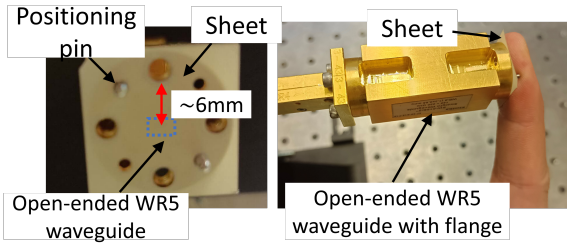


Fig. 4. The setup of finger permittivity measurement.

our measurements, the fingers under consideration were not washed or dried to maintain a typical daily humidity level encountered during mobile terminal usage. In the context of finger-antenna interactions, particularly during mobile terminal usage, it is the fingerprint sides that notably influence the radiation patterns of the mobile terminal antennas. Therefore, the measurements primarily focus on the fingerprint sides, while the fingernail sides are not considered.

Additionally, different parts of the fingers, especially the fingerprint regions, may show varying permittivities. Hence, averaging permittivity estimates from multiple finger measurements is essential for obtaining representative values. To collect finger permittivity estimates across various

individuals, we conducted measurements with 10 volunteer subjects aged between 18 and 40 years old. Each volunteer underwent 10 measurements, focusing on the fingertips of their index, middle, and ring fingers.

IV. RESULTS AND DISCUSSIONS

The mean of the estimated relative permittivities is depicted in Fig. 5a for each volunteer. For instance, at 140 GHz, the dielectric constant (real part) ranges from 3.9 to 5.9, while the loss factor (imaginary part) varies from 1.9 to 3.9. In most cases, the dielectric constants fall within the range of 3.9 to 4.8, while the loss factors fall between 1.9 to 2.4. The average relative permittivity of all volunteers is $\epsilon_r = 4.7 - 2.4i$ at 140 GHz. It can be seen that Volunteer 7 and 8 show higher dielectric constants and loss factors at 140 GHz and show different trends with frequency changes. This is because these two volunteers' hands are more moist.

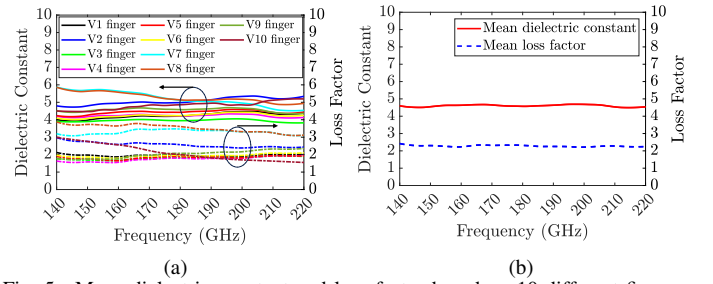


Fig. 5. Mean dielectric constant and loss factor based on 10 different finger parts for a) each volunteer and b) all the volunteers.

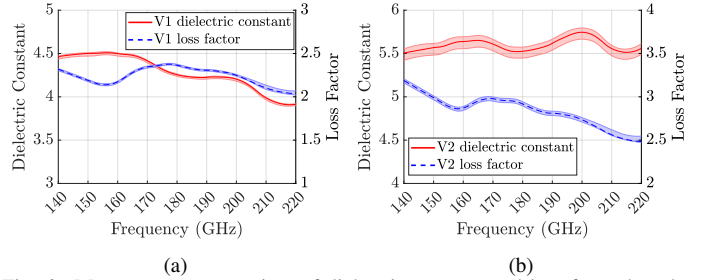


Fig. 6. Measurement uncertainty of dielectric constant and loss factor based on 20 measurements at the same finger location for a) Volunteer 1 and b) Volunteer 2.

To assess measurement uncertainty, 20 repeated measurements were conducted within a short duration of 2 minutes at the same finger location of two volunteers. The estimated relative deviation of permittivity is within $\pm 1.4\%$ of the mean value for the dielectric constants and within $\pm 1.2\%$ for loss factors, as presented in Fig. 6. These relative deviations are smaller than those reported in [10], indicating the high repeatability of the measurement method. Additionally, a variation in permittivity for each volunteer was observed based on the 10 measurements on different finger parts as shown in Fig. 7. The majority of volunteers' fingers exhibit a variation of < 1 for both the dielectric constants and loss factors. Some volunteers' dielectric constants show a larger variation, like Fig. 7d, 7e, and 7g, while some others show a larger variation in loss factors, like Fig. 7b, 7c, and 7h.

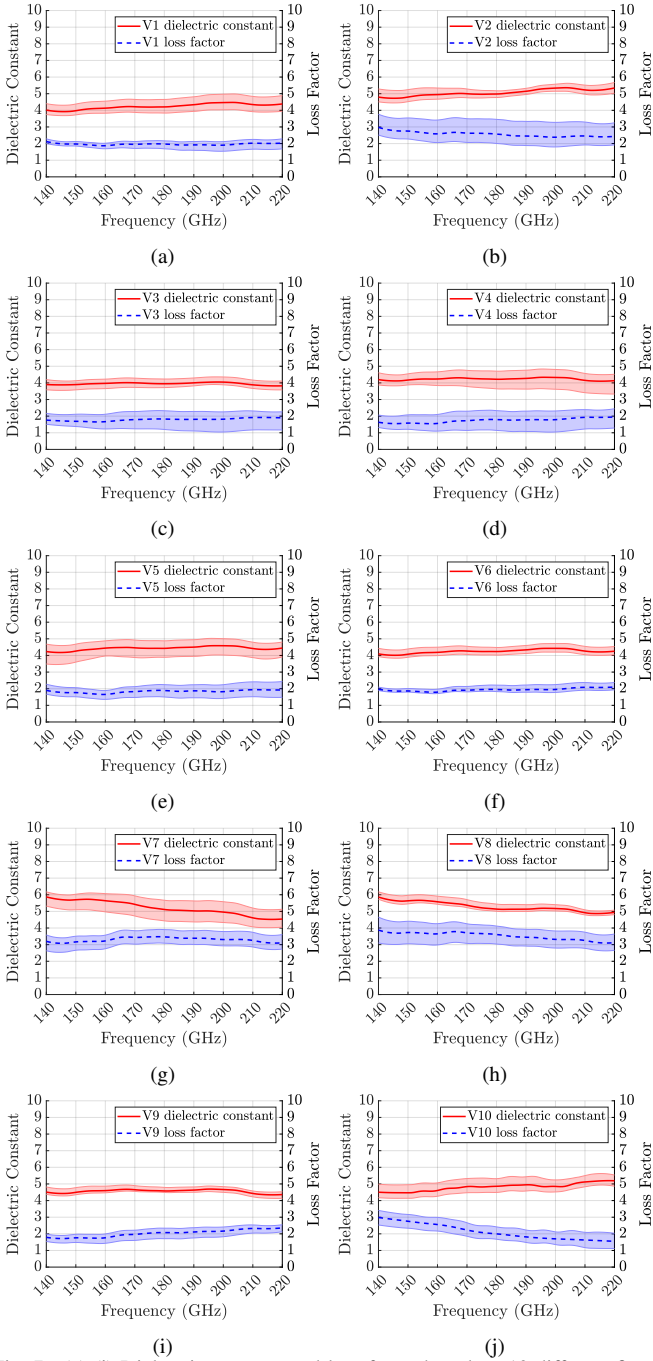


Fig. 7. (a)-(j) Dielectric constant and loss factor based on 10 different finger parts for 10 volunteers.

V. CONCLUSIONS

In this paper, we propose a novel method for characterizing human skin permittivity using an open-ended waveguide at sub-THz frequencies. The necessary contact area of the human skin under test on the sheet is identified through full-wave simulations so that the antenna-hand interaction model can excellently emulate practical measurements. The full-wave simulations provide reflection coefficients to train the RBN, which is applied to characterize finger permittivities of living humans. The estimated relative permittivity shows smaller uncertainty than $\pm 1.4\%$ for both

the dielectric constants and loss factors, demonstrating the high repeatability of the proposed approach. The measured complex relative permittivity estimates are valuable base for studying finger-antenna interactions of sub-THz mobile handsets. Furthermore, the proposed method can be applied to characterize the permittivity of various parts of human skin.

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