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Research Articles: Behavioral/Cognitive

## Cortical tracking of speech-in-noise develops from childhood to adulthood

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# Cortical tracking of speech-in-noise develops from childhood to adulthood

**Abbreviated Title:** Cortical processing of speech-in-noise in children

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**Conflict of interest**

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1 **Abstract**

2 In multitalker backgrounds, the auditory cortex of adult humans tracks the attended  
3 speech stream rather than the global auditory scene. Still, it is unknown whether such  
4 preferential tracking also occurs in children whose speech-in-noise (SiN) abilities are  
5 typically lower compared with adults.

6 We used magnetoencephalography (MEG) to investigate the frequency-specific cortical  
7 tracking of different elements of a cocktail-party auditory scene in twenty children (6–9 years;  
8 8 females) and twenty adults (21–40 years; 10 females). During MEG recordings, subjects  
9 attended to 4 different 5-min stories, mixed with different levels of multitalker background at  
10 four signal-to-noise ratios (SNRs: noiseless, +5, 0, and –5 dB). Coherence analysis quantified  
11 the coupling between the time courses of the MEG activity and attended speech stream,  
12 multitalker background or global auditory scene, respectively.

13 In adults, statistically significant coherence was observed between MEG signals  
14 originating from the auditory system and the attended stream at < 1 Hz, 1–4 Hz, and 4–8 Hz  
15 in all SNR conditions. Children displayed similar coupling at < 1 Hz and 1–4 Hz, but  
16 increasing noise impaired the coupling more strongly than in adults. Also, children displayed  
17 drastically lower coherence at 4–8 Hz in all SNR conditions.

18 These results suggest that children's difficulties to understand speech in noisy  
19 conditions are related to an immature selective cortical tracking of the attended speech  
20 streams. Our results also provide unprecedented evidence for an acquired cortical tracking of  
21 speech at syllable-rate and argue for a progressive development of SiN abilities in humans.

22 **Significance statement:**

23 Behaviorally, children are worse than adults at understanding speech-in-noise. Here,  
24 neuromagnetic signals were recorded while healthy adults and typically developing 6–9-year-  
25 old children attended to a speech stream embedded in a multitalker background noise with  
26 varying intensity. Results demonstrate that auditory cortices of both children and adults  
27 selectively track the attended speaker’s voice rather than the global acoustic input at phrasal  
28 and word rates. However, increments of noise compromised the tracking significantly more in  
29 children than in adults. Unexpectedly, children displayed limited tracking of both the attended  
30 voice and the global acoustic input at the 4–8-Hz syllable rhythm. Thus, both speech-in-noise  
31 abilities and cortical tracking of speech syllable repetition rate seem to mature later in  
32 adolescence.

33

34

## 35 Introduction

36  
37 Children often grow up and learn in noisy surroundings. Clamorous classrooms, rowdy  
38 playgrounds, and domestic sound disturbances indeed constitute adverse auditory scenes for a  
39 still immature auditory system.

40 Interestingly, speech-in-noise (SiN) perception in children appears strenuous but  
41 improves during late childhood ( $\geq 10$  years) due to maturation of the auditory system and  
42 attentional abilities (Elliott, 1979; Moore et al., 2010; Sanes and Woolley, 2011; Thompson et  
43 al., 2017). Still, the neurophysiological mechanisms accounting for the improvement in SiN  
44 perception observed from childhood to adulthood are unsettled. It has been hypothesized that,  
45 in adverse auditory scenes, children's auditory system would actually lack the capacity to  
46 segregate the attended auditory stream from the unattended noisy background (Sanes and  
47 Woolley, 2011). However, no study has so far demonstrated such phenomena in children.

48 Accumulating evidence shows that adults' auditory system tracks the attended speech  
49 stream rather than the global auditory scene in a multitalker background (Mesgarani and  
50 Chang, 2012). In such adverse auditory background, the auditory system entrains to the slow  
51 amplitude modulations (i.e., the temporal envelope) of the attended speaker's voice rather  
52 than to modulations of the global auditory scene (Ding and Simon, 2012a; Zion Golumbic et  
53 al., 2013; Vander Ghinst et al., 2016). This coupling typically occurs at frequencies below 10  
54 Hz and declines with increasing noise level. Given that this frequency range matches with  
55 prosodic stress/phrasal/sentential ( $< 1$  Hz), word (1–4 Hz), and syllable (4–8 Hz) repetition  
56 rates, the corresponding cortical tracking of speech has been hypothesized to subserve the  
57 chunking of the continuous verbal flow into relevant segments used for further speech  
58 recognition, up to a certain noise level (Ding and Simon, 2012a; Giraud and Poeppel, 2012;  
59 Ding and Simon, 2013a; Vander Ghinst et al., 2016; Keitel et al., 2018).

60        How children's auditory system tracks connected speech has remained largely  
61 unknown. Until now, cortical tracking of speech in children has only involved dyslexic  
62 children older than 11 years, showing that they have impaired tracking below 2 Hz compared  
63 with age-matched healthy control subjects (Molinaro et al., 2016; Power et al., 2016).  
64 However, to the best of our knowledge, no study has so far investigated how this low-  
65 frequency cortical tracking might differ between typically developed children and adults, and  
66 whether noise differentially corrupts the coupling in these two populations. We therefore  
67 specifically test the hypothesis that children's poor SiN perception abilities (Elliott, 1979;  
68 Berman and Friedman, 1995) are related to inaccurate low-frequency cortical tracking of the  
69 attended speech stream in a noisy background.

70        To test this hypothesis, children (6–9 years) and adults (21–40 years) with normal SiN  
71 perception listened to speech recordings mixed with a cocktail party noise at different  
72 intensities in an ecological connected speech listening paradigm. Based on  
73 magnetoencephalographic (MEG) recordings, we quantified the cortical tracking of the  
74 different elements of the auditory scene: (i) *Attended stream* (i.e., reader's voice only), (ii)  
75 unattended *Multitalker background* only, and (iii) *Global scene* (i.e., the combination of the  
76 *Attended stream* and the unattended *Multitalker background*).

## 77 **Methods**

78 The methods used for MEG data acquisition, preprocessing, and analyses are derived from  
79 previous studies (Bourguignon et al., 2013; Vander Ghinst et al., 2016).

## 81 ***Participants***

82 Twenty native French-speaking healthy children (mean age 8 yrs, range 6–9 yrs; 8  
83 females and 12 males) and twenty native French-speaking healthy adults (mean age 30 yrs,  
84 range 21–40 yrs; 10 females and 10 males) without any history of neuropsychiatric or  
85 otologic disorder participated in this study. All subjects had normal hearing according to pure  
86 tone audiometry (i.e., normal hearing thresholds (between 0–20 dB HL) for 250, 500, 1000,  
87 2000, 4000, and 8000 Hz) and normal otomicroscopy. Subjects' auditory perception was  
88 assessed with three separate subtests of a validated and standardized French language central  
89 auditory battery: 1) a dichotic test, 2) a speech audiometry, and 3) a SiN audiometry  
90 (Demanez et al., 2003). In the two later tests, 30 monosyllabic words were presented with (3)  
91 or without (2) noise in a predetermined counterbalanced order, so that every word is presented  
92 once in silence, and once in noise. A score was then obtained, corresponding to the number of  
93 words correctly repeated with and without noise. According to the tests (1–3), all subjects had  
94 normal dichotic perception, speech and SiN perception for their age (Demanez et al., 2003).  
95 Children and adults were all right-handed according to the Edinburgh handedness inventory  
96 (Oldfield, 1971). The study had prior approval by the ULB-Hôpital Erasme Ethics  
97 Committee. Participants gave written informed consent before participation.

## 99 ***Experimental paradigm***

100 During MEG recordings, the subjects sat comfortably in the MEG chair with the arms  
101 resting on a table positioned in front of them. They underwent four listening conditions and

102 one rest condition, each lasting five minutes. The order of the five conditions was randomized  
103 for each subject.

104       Subjects were told before the task that questions on the content of the story would be  
105 asked after each listening condition. Children were given a clue about the content of the text  
106 they were about to listen to ensure that they selected the attended auditory stream  
107 straightaway (e.g., “you are going to listen to the story of two little princes”). During the  
108 listening conditions, subjects listened to four different stories in French recorded by different  
109 native adult French-speakers. The recordings were randomly selected from a set of four  
110 stories (readers’ sex ratio: 1/1) obtained from a French audiobook database  
111 (<http://www.litteratureaudio.com>) after written authorization from the readers. Children and  
112 adults listened to different stories adapted to their age to maximize their implication in the  
113 task, and their comprehension of the stories. This approach was particularly important for  
114 stories used in children as it has been previously demonstrated that reading stories aloud from  
115 books exposes children to a linguistic and cognitive complexity typically not found in child-  
116 directed or adult-directed speech (Massaro, 2017). Special care was therefore taken to select  
117 stories with comprehensible vocabulary and content. Phrasal, word, and syllable rates,  
118 assessed as the number of phrases, words, or syllables divided by the corrected duration of the  
119 audio recording, were comparable in children (mean phrasal, word and syllable rates across  
120 different stories 0.45 Hz, 3.6 Hz, and 5.54 Hz) and in adults (0.49 Hz, 3.39 Hz, and 5.56 Hz,  
121 respectively). For phrases, the corrected duration was (trivially) the total duration of the audio  
122 recording. For words and syllables, the corrected duration was the total time during which the  
123 speaker was actually speaking, that is the total duration of the audio recording (here 5 min)  
124 minus the sum of all silent periods when the speech amplitude was below a tenth of the mean  
125 amplitude for at least 10 ms. A specific speech signal-to-noise ratio (SNR; where signal was  
126 attended reader's voice, and noise was the multi-talker background) was randomly assigned to

each story: a noiseless condition, and 3 SiN conditions (with SNRs of +5 dB, 0 dB, and –5 dB), leading to four different SNR conditions. This randomization procedure prevented any systematic association between stories and SNRs. The noise (Fonds sonores v-1.0, Perrin & Grimault 2005) was a continuous cocktail party noise obtained by mixing the voices of six native French speakers talking simultaneously in French (three females and three males). This configuration of cocktail-party noise was selected because it accounts for both energetic and informational masking at phonetic and lexical level (Simpson and Cooke, 2005; Hoen et al., 2007). Sound recordings were played using VLC media player (VideoLAN Project, GNU General Public License) running on a MacBook Pro (Apple Computer, Inc., Cupertino, CA). Sound signals were transmitted to a MEG-compatible  $60 \times 60 \text{ cm}^2$  high-quality flat panel loudspeaker (Panphonics SSH sound shower, Panphonics Oy, Espoo, Finland) placed 2.4 m away in front of the subjects. The average sound intensity was set to 60 dB as assessed by a sound level meter (Sphynx Audio System, Belgium). Subjects were asked to attend to the reader's voice and to gaze at a fixation point on the wall of the magnetically shielded room facing them. During the *Rest* condition, subjects were instructed to relax, not to move, and to gaze at the same fixation point. At the end of each listening condition, subjects were asked to score the intelligibility of the attended reader's voice on a visual analog scale (VAS) ranging from 0 to 10 (0 = totally unintelligible; 10 = perfectly intelligible) and were also asked (adults) or 8 (children) yes/no forced-choice questions exploring the salience and explicitness of the heard story by analogy with what is required for the clinical diagnosis of text comprehension deficits (Ferstl et al., 2005).

#### ***Data acquisition***

Cortical neuromagnetic signals were recorded at ULB-Hôpital Erasme using a whole-scalp-covering 306-channel MEG device (for 15 adults and 12 children Elekta Neuromag

Vectorview by Elekta Oy, Helsinki, Finland, and otherwise Elekta Neuromag Triux by MEGIN, Helsinki, Finland) installed in a light-weight magnetically shielded room (Maxshield, MEGIN, Helsinki, Finland), the characteristics of which being described elsewhere (De Tiège et al., 2008; Carrette et al., 2011). The MEG device has 102 sensor chipsets, each comprising one magnetometer and two orthogonal planar gradiometers. MEG signals were bandpass-filtered through 0.1–330 Hz and sampled at 1 kHz. Four head-tracking coils monitored subjects' head position inside the MEG helmet. The locations of the coils and at least 150 head-surface (on scalp, nose, and face) points with respect to anatomical fiducials were digitized with an electromagnetic tracker (Fastrack, Polhemus, Colchester, VT). Electro-oculogram (EOG), electrocardiogram (ECG), and the audio signals presented to the subjects were recorded simultaneously with MEG signals (passband 0.1–330 Hz for EOG and ECG, and low-pass at 330 Hz for audio signals). The recorded audio signals were used for synchronization between MEG and the transmitted audio signals, the latter being bandpass-filtered at 50–22000 Hz and sampled at 44.1 kHz. High-resolution 3D-T1 cerebral magnetic resonance images (MRI) were acquired on a 1.5 T MRI (Intera, Philips, The Netherlands).

#### ***Data preprocessing***

Continuous MEG data were first preprocessed off-line using the temporal extension of the signal-space-separation method (correlation limit, 0.9; segment length, 20 s) to suppress external inferences and correct for head movements (Taulu et al., 2005; Taulu and Simola, 2006). For the subsequent coherence analyses used to quantify the cortical tracking of speech, continuous MEG and audio signals were split into 2048-ms epochs with 1638-ms epoch overlap, leading to a frequency resolution of ~0.5 Hz (Bortel and Sovka, 2007). MEG epochs exceeding 3 pT (magnetometers) or 0.7 pT/cm (gradiometers) were excluded from further analysis to avoid contamination of the data by eye movement artifacts, muscle activity, or



artifacts in the MEG sensors. The number of artifact-free epochs was  $695 \pm 66$  (mean  $\pm$  SD across subjects and conditions) in the adult group and  $621 \pm 93$  in the children group.

A two-way repeated-measures ANOVA (factors: age group and condition; dependent variable: number of epochs used to compute coherence) revealed a significant effect of group on the number of epochs ( $F_{1,114} = 4.42$ ,  $p = 0.042$ ) but no effect of SNR ( $F_{3,114} = 0.03$ ,  $p = 0.99$ ) or interaction ( $F_{3,114} = 1.46$ ,  $p = 0.23$ ). To avoid a possible methodological bias in our results due to differences between age groups in the accuracy of speech tracking estimation, we threw away epochs in adults' data so as to equalize the number of epochs in both groups.

#### *Coherence analyses in sensor space*

For each listening condition, synchronization between the temporal envelope of wide-band (50–22000 Hz) audio signals and artifact-free MEG epochs (2048-ms-long) was assessed with coherence analysis in sensor space at frequencies in which speech temporal envelope is critical for speech comprehension (i.e., 0.1–20 Hz) (Drullman et al., 1994). Coherence is an extension of Pearson correlation coefficient to the frequency domain. It quantifies the degree of coupling between two signals (say  $x(t)$  and  $y(t)$ ), providing a number between 0 (no linear dependency) and 1 (perfect linear dependency) for each frequency bin (Halliday et al., 1995). Coherence was computed as follows:

$$\text{Coh}_{xy}(f) = \frac{|P_{xy}(f)|^2}{P_{xx}(f)P_{yy}(f)},$$

where  $P_{xx}(f) = \sum_k |\hat{x}_k(f)|^2$ ,  $P_{yy}(f) = \sum_k |\hat{y}_k(f)|^2$ , and  $P_{xy}(f) = \sum_k |\hat{x}_k(f)\hat{y}_k^*(f)|$ , and where  $\hat{x}_k(f)$  (respectively  $\hat{y}_k(f)$ ) is the Fourier coefficient of the  $k^{\text{th}}$  epoch of signal  $x(t)$  (respectively  $y(t)$ ) at frequency bin  $f$ , and  $*$  denotes the complex conjugate. In our

199 application, coherence analysis provides a quantitative assessment of the cortical tracking of  
200 speech.

201 For the three SiN conditions (+5 dB, 0 dB, and -5 dB), coherence was separately  
202 computed between MEG signals and three acoustic elements of the auditory scene: 1) the  
203 *Global scene (Attended stream + Multitalker background)*, leading to  $Coh_{global}$ , 2) the  
204 *Attended stream* only (i.e., the reader's voice), leading to  $Coh_{att}$ , and 3) the *Multitalker*  
205 *background* only, leading to  $Coh_{bckgr}$ . Sensor-level coherence maps were obtained using  
206 gradiometer signals only, and signals from gradiometer pairs were combined as done in  
207 Bourguignon et al. (2015).

208 Previous studies have demonstrated statistically significant coupling between acoustic  
209 and brain signals at frequencies corresponding to phrases, words, and syllables (Ding and  
210 Simon, 2012b; Bourguignon et al., 2013; Peelle et al., 2013; Clumeck et al., 2014; Koskinen  
211 and Seppä, 2014; Vander Ghinst et al., 2016; Keitel et al., 2018). Accordingly, sensor-level  
212 coherence maps were produced separately for phrases (frequency bin corresponding to 0.5  
213 Hz), words (average across the frequency bins falling in 1–4 Hz) and syllables (4–8 Hz). Note  
214 that coherence at the frequency bin corresponding to 0.5 Hz actually reflects coupling in a  
215 frequency range around 0.5 Hz, with a sensitivity profile proportional to the Fourier transform  
216 of a boxcar function:  $\text{sinc}(\pi(f-0.5 \text{ Hz})/0.5 \text{ Hz})$ . The < 1 Hz, 1–4 Hz, and 4–8 Hz frequency  
217 ranges are henceforth referred to as *frequency bands of interest*.

218

### 219 ***Coherence analyses in source space***

220 Individual MRIs were first segmented using Freesurfer software (Martinos Center for  
221 Biomedical Imaging, Boston, MA, RRID:SCR\_001847; (Reuter et al., 2012)). MEG and  
222 segmented MRI coordinate systems were then coregistered using the three anatomical fiducial  
223 points for initial estimation and the head-surface points to manually refine the surface

coregistration. The MEG forward model was computed for triplets of orthogonal current dipoles, placed on a homogenous 5-mm-grid source space covering the whole brain, using MNE suite (Martinos Centre for Biomedical Imaging, Boston, MA, RRID:SCR\_005972; (Gramfort et al., 2014)). The forward model was then reduced to its two first principal components. This procedure is justified by the insensitivity of MEG to currents radial to the skull, and hence, this dimension reduction leads to considering only the tangential sources. As a preliminary step, to simultaneously combine data from planar gradiometers and magnetometers for source estimation, sensor signals (and the corresponding forward-model coefficients) were normalized by their noise root mean square, estimated from the *Rest* data filtered through 1–195 Hz. Coherence maps obtained for each subject, listening condition (*Noiseless*, +5 dB, 0 dB, and –5 dB), audio signal (*Global scene*, *Attended stream*, *Multitalker Background*) and frequency bands of interest (< 1 Hz, 1–4 Hz, and 4–8 Hz) were finally produced using the Dynamic Imaging of Coherent Sources approach (Gross et al., 2001) with Minimum-Norm Estimates inverse solution (Dale and Sereno, 1993). Noise covariance was estimated from the *Rest* data filtered through 1–195 Hz and the regularization parameter was fixed in terms of MEG sensor noise level as done by Hämäläinen et al. (2010).

#### ***Group-level analyses in source space***

A non-linear transformation from individual MRIs to the standard Montreal Neurological Institute (MNI) brain was first computed using the spatial normalization algorithm implemented in Statistical Parametric Mapping (SPM8, Wellcome Department of Cognitive Neurology, London, UK, RRID:SCR\_007037; (Ashburner et al., 1997; Ashburner and Friston, 1999)) and then applied to individual MRIs and every coherence map. The adult MNI template was used in both children and adults despite the fact that spatial normalization may fail for brains of small size when using an adult template (Reiss et al., 1996). However,

249 this risk is negligible for the population studied here. Indeed, the brain volume does not  
 250 change substantially from the age of 5 years to adulthood (Reiss et al., 1996). This assumption  
 251 has been confirmed by a study that specifically addressed this question in children aged above  
 252 6 years (Muzik et al., 2000).

253 To produce coherence maps at the group level, we computed across subjects the  
 254 generalized  $f$ -mean of normalized maps, according to  $f(\cdot) = \text{arctanh}(\sqrt{\cdot})$ , namely, the Fisher  
 255  $z$ -transform of the square-root. This procedure transforms the noise on the coherence estimate  
 256 into an approximately normally distributed noise (Rosenberg et al., 1989). Thus, the  
 257 computed coherence is an unbiased estimate of the mean coherence at the group-level. In  
 258 addition, this averaging procedure avoids an over-contribution of subjects characterized by  
 259 high coherence values to the group analysis (Bourguignon et al., 2012). The resulting subject-  
 260 and group-level coherence maps are henceforth referred to as the *audio* maps.

261

## 262 *Experimental design and statistical analyses*

263 Sample size was based on a previous study from our group with a similar design, which  
 264 included 20 healthy adults (Vander Ghinst et al., 2016). Accordingly, we set the sample size  
 265 to 20 per age group.

266

## 267 *Comparison of SiN perception in adults vs. children*

268 Children' and adults' capacities to understand speech and SiN—as measured with  
 269 speech and SiN audiometry—were compared with a  $t$ -test.

270

## 271 *Effect of SNR on the comprehension and the intelligibility of the Attended stream.*

272 A two-way repeated-measures ANOVA was used to assess the effects of the multitalker  
 273 background noise level (within-subject factor; *Noiseless*,  $+5$  dB,  $0$  dB, and  $-5$  dB) and of the

274 age group (between-subjects factor; adults, children) on the comprehension scores and  
 275 intelligibility ratings separately. The distribution of the residues of the ANOVAs was then  
 276 tested for normality using the Lilliefors test (Lilliefors, 1967).

277 Of note, we acknowledge that the interpretability of these analyses could be limited for  
 278 two reasons. First, adults and children listened to different texts and had to answer questions  
 279 where the difficulty was adapted to their age. Second, the intelligibility ratings by children  
 280 and adults may differ also due to differences in the visual analogue scales: explicit visual  
 281 support was provided for the children (more or less happy faces) to facilitate the evaluation.

282

283

#### 284 *Significance of individual subjects' coherence values*

285 The statistical significance of individual subjects' coherence values (for each listening  
 286 condition, audio signal, and frequency band of interest) was assessed with surrogate-data-  
 287 based maximum statistics. This statistical assessment was performed on sensor-space  
 288 coherence values, and it tested the null hypothesis that the brain does not track audio signals  
 289 more than other plausible unrelated (surrogate) signals. This method was chosen because it  
 290 intrinsically deals with the issue of multiple-comparisons across sensors, and as it takes into  
 291 account the temporal auto-correlation within signals. For each subject, 1000 surrogate sensor-  
 292 level coherence maps were computed as done for genuine coherence maps but with audio  
 293 signals replaced by Fourier transform surrogate audio signals (Faes et al., 2004). The  
 294 maximum coherence value across all sensors was extracted for each surrogate simulation, and  
 295 the 95<sup>th</sup> percentile of this distribution of maximum coherence values yielded the significance  
 296 threshold at  $p < 0.05$ .

297

#### 298 *Significance of group-level coherence values*

299 The statistical significance of coherence values in group-level *audio* maps was  
 300 assessed for each hemisphere separately with a non-parametric permutation test (Nichols and  
 301 Holmes, 2002). In practice, subject- and group-level *Rest* coherence maps were computed as  
 302 done for the *audio* maps, but with MEG signals in listening conditions replaced by *Rest* MEG  
 303 signals and sound signals unchanged. Group-level difference maps were obtained by  
 304 subtracting *f*-transformed *audio* and *Rest* group-level coherence maps. Under the null  
 305 hypothesis that coherence maps are the same whatever the experimental condition, the  
 306 labeling *audio* and *Rest* are exchangeable at the subject-level prior to group-level difference  
 307 map computation (Nichols and Holmes, 2002). To reject this hypothesis and to compute a  
 308 threshold of statistical significance for the correctly labeled difference map for each  
 309 hemisphere separately, the permutation distribution of the maximum of the difference map's  
 310 absolute value in each hemisphere was computed for 10,000 permutations. The test assigned a  
 311 *p* value to each voxel in the group-level *audio* map, equal to the proportion of surrogate  
 312 values exceeding the corresponding voxel's difference value (Nichols and Holmes, 2002).

313 We further identified the coordinates of local maxima in group-level coherence maps.  
 314 Such local coherence maxima are sets of contiguous voxels displaying higher coherence  
 315 values than all neighbouring voxels. We only report statistically significant local coherence  
 316 maxima, disregarding the extents of these clusters. Indeed, cluster extent is hardly  
 317 interpretable in view of the inherent smoothness of MEG source reconstruction (Hämäläinen  
 318 et al., 1994; Wens et al., 2015; Bourguignon et al., 2017).

319

#### 320 *Cortical processing of the auditory scene in SiN conditions*

321 To identify cortical areas wherein activity reflects more the *Attended stream* than the  
 322 *Global scene*, we compared  $Coh_{att}$  to  $Coh_{global}$  maps using the same non-parametric

323 permutation test described above, but with the labels *Global scene* and *Attended stream*  
 324 instead of *audio* and *Rest*, leading to the  $Coh_{att} - Coh_{global}$  difference maps.

325

326 *Comparison of the tracking in adults vs. children*

327 To identify cortical areas showing stronger tracking in adults than children (and vice  
 328 versa), we compared the corresponding coherence maps using the above described  
 329 permutation test, but with the labels  $Coh_{att,adults}$  and  $Coh_{att,children}$  instead of  $Coh_{att}$  and  
 330  $Coh_{global}$ , leading to the  $Coh_{att,adults} - Coh_{att,children}$  difference maps.

331

332 *Effect of the SNR, age group, and hemispheric lateralization on cortical tracking of speech in*  
 333 *noise*

334 In this between-subject design, we used a 3-way repeated-measures ANOVA to  
 335 compare cortical tracking of speech between  $n = 20$  children and  $n = 20$  adults with additional  
 336 factors of hemisphere (left vs. right) and four different SNR conditions (*Noiseless*,  $+5$  dB,  $0$   
 337 dB, and  $-5$  dB). The dependent variable was the maximal  $Coh_{att}$  value within a sphere of 10  
 338 mm radius around the maximum of the group-level difference map in each hemisphere. As  
 339 the Lilliefors test revealed that the distribution of the residues of the ANOVAs deviated  
 340 statistically significantly from the normal distribution for 1–4 Hz and 4–8 Hz  $Coh_{att}$  values ( $ps$   
 341  $< 0.05$ ), we repeated the ANOVAs on the coherence values transformed with the  
 342 transformation used to average source coherence maps ( $f(\cdot) = \text{arctanh}(\sqrt{\cdot})$ ). After such  
 343 transformation, the residues did not deviate significantly from a normal distribution ( $ps >$   
 344  $0.05$ ). Therefore, we report on only the results of the later ANOVAs. Post-hoc comparisons  
 345 were performed with pairwise t-tests.

346       Based on our results in the *Noiseless* condition, we conducted an additional analysis by  
347   computing Pearson correlation between children's age and their maximum coherence values,  
348   separately for both hemispheres in the three frequency bands of interest.

349

350

351

352



## 353 Results

354

355 In this study, children and adults were listening to connected speech embedded in a  
 356 multitalker background with different SNR conditions. Ensuing cortical tracking of speech  
 357 (i.e., the coupling between brain activity and audio signals) was quantified with coherence  
 358 analysis. The specific aim was to compare this tracking between children and adults.

359

### 360 *Comparison of SiN perception in adults vs. children*

361 Speech perception in silence did not differ ( $t_{38} = 1.27$ ;  $p = 0.211$ ) between children  
 362 ( $28.35 \pm 0.88$ ; mean  $\pm$  SD) and adults ( $28.7 \pm 0.86$ ). SiN perception quantified with SiN  
 363 audiometry was significantly ( $t_{38} = 3.35$ ;  $p = 0.0018$ ) poorer in children ( $25.75 \pm 1.33$ ) than in  
 364 adults ( $27.1 \pm 1.21$ ).

365

### 366 *Effect of SNR on the comprehension and the intelligibility of the Attended stream*

367 Figure 1 displays the comprehension scores and intelligibility ratings in the different  
 368 SNR conditions in both groups.

369 In the *Noiseless* condition, all adult participants gave the maximum intelligibility rating  
 370 (10), leading to a null variance. For this reason, the ANOVA for the intelligibility ratings was  
 371 computed only with the 3 other conditions ( $+5$  dB,  $0$  dB, and  $-5$  dB). Doing otherwise would  
 372 have violated the homoscedasticity assumption of the ANOVA.

373 The ANOVA performed on intelligibility rating revealed a statistically significant effect  
 374 of SNR ( $F_{2,76} = 119$ ;  $p < 0.0001$ ), and a significant interaction between SNR and age-group  
 375 ( $F_{2,76} = 4.94$ ;  $p = 0.0096$ ), but no significant effect of age group ( $F_{1,38} = 0.05$ ;  $p = 0.83$ ). The  
 376 Lilliefors test showed that the distribution of the residuals did not deviate significantly from a  
 377 normal distribution ( $p = 0.15$ ). Post hoc comparisons performed with pairwise  $t$ -tests between  
 378 adjacent conditions demonstrated that intelligibility rating decreased statistically significantly

379 from *Noiseless* to +5 dB (adults,  $t_{19} = 6.28$ ,  $p < 0.0001$ ; children,  $t_{19} = 5.06$ ,  $p < 0.0001$ ), from  
 380 +5 dB to 0 dB (adults,  $t_{19} = 7.19$ ,  $p < 0.0001$ ; children,  $t_{19} = 2.11$ ,  $p = 0.048$ ) and from 0 dB to  
 381 -5 dB (adults,  $t_{19} = 9.48$ ,  $p < 0.0001$ ; children,  $t_{19} = 5.09$ ,  $p < 0.0001$ ). Comparison between  
 382 adults and children revealed that children gave lower intelligibility ratings than adults in  
 383 Noiseless ( $t_{38} = 2.26$ ,  $p = 0.030$ ) and +5 dB conditions ( $t_{38} = 2.10$ ,  $p = 0.042$ ) but not in the  
 384 two other noisiest conditions ( $ps > 0.05$ ).

385 The ANOVA performed on comprehension scores—converted to percentage correct—  
 386 revealed a significant effect of SNR ( $F_{3,114} = 27.6$ ;  $p < 0.0001$ ), a significant effect of age  
 387 group ( $F_{1,38} = 19.4$ ;  $p < 0.0001$ ), and no significant interaction ( $F_{3,114} = 0.66$ ;  $p = 0.58$ ). The  
 388 Lilliefors test showed that the distribution of the residuals did not deviate significantly from a  
 389 normal distribution ( $p = 0.054$ ). Comprehension scores were higher in adults ( $80.5 \pm 15.2$  %;  
 390 mean  $\pm$  SD across conditions and participants) than in children ( $68.6 \pm 18.7$  %), and  
 391 decreased statistically significantly from *Noiseless* to +5 dB ( $t_{39} = 3.13$ ,  $p = 0.0033$ ), from +5  
 392 dB to 0 dB ( $t_{39} = 2.13$ ,  $p = 0.040$ ) and from 0 dB to -5 dB ( $t_{39} = 4.00$ ,  $p = 0.0003$ ).

393  
 394 ---Place Figure 1 around here ---

### 396 397 ***Cortical tracking of speech in the Noiseless condition***

398 Figures 2–4 display group-averaged coherence spectra (Fig. 2), sensor distribution (Fig.  
 399 3) and source distribution (Fig. 4) in all conditions and in both groups.

400 Table 1 provides the number of children and adults showing significant sensor-space  
 401  $Coh_{global}$ ,  $Coh_{att}$ , and  $Coh_{bckgr}$  at <1 Hz, 1–4 Hz and 4–8 Hz frequencies.

402 In adults, statistically significant  $Coh_{att}$  was observed at < 1 Hz in 20/20 adults, at 1–4  
 403 Hz in 17/20 adults, and at 4–8 Hz in 17/20 adults in temporal-lobe MEG sensors in the  
 404 *Noiseless* condition (Figs. 2 and 3). In source space, group-level coherence at <1 Hz peaked at

405 bilateral superior temporal sulcus (STS; left-hemisphere MNI coordinates  $[-66 \ -16 \ -1]$ ,  $p <$   
 406  $0.0001$ ; right  $[66 \ -26 \ 5]$ ,  $p < 0.0001$ ), left inferior frontal gyrus (IFG;  $[-61 \ -6 \ 34]$ ,  $p =$   
 407  $0.0037$ ) and right central sulcus ( $[59 \ -5 \ 41]$ ,  $p = 0.034$ ). In addition,  $Coh_{att}$  peaked in  
 408 bilateral supratemporal auditory cortices (AC) at 1–4 Hz (left  $[-65 \ -16 \ 7]$ ,  $p < 0.0001$ ; right  
 409  $[64 \ -5 \ 6]$ ,  $p < 0.0001$ ) and 4–8 Hz (left  $[-65 \ -15 \ 9]$ ,  $p < 0.0001$ ; right  $[64 \ -8 \ 5]$ ,  $p <$   
 410  $0.0001$ ) (Fig. 4).

411 In children, statistically significant  $Coh_{att}$  was observed at  $< 1$  Hz in 20/20 children, at  
 412 1–4 Hz in 10/20 children, and at 4–8 Hz in 11/20 children in temporal-lobe MEG sensors in  
 413 the *Noiseless* condition (Figs. 2 and 3). In source space, group-level coherence at  $< 1$  Hz  
 414 peaked at bilateral STS (left  $[-63 \ -10 \ 6]$ ,  $p < 0.0001$ ; right  $[63 \ -20 \ -3]$ ,  $p < 0.0001$ ). It  
 415 peaked at bilateral supratemporal AC at 1–4 Hz (left  $[-64 \ -11 \ 13]$ ,  $p = 0.0016$ ; right  $[62 \ -28$   
 416  $4]$ ,  $p < 0.0001$ ), and in left supratemporal AC at 4–8 Hz ( $[-65 \ -17 \ 10]$ ,  $p = 0.018$ ). Of note,  
 417 coherence did peak in the right supratemporal AC at 4–8 Hz but this local maximum did not  
 418 reach statistical significance ( $[64 \ -14 \ 5]$ ,  $p = 0.11$ ).

419 The above results suggest that speech tracking differed somewhat in adults and children  
 420 at 1–4 Hz and 4–8 Hz but not at  $< 1$  Hz. Indeed, a smaller proportion of children than of  
 421 adults showed significant tracking at 1–4 Hz (10/20 vs. 17/20;  $p = 0.041$ ; Fisher exact test). A  
 422 similar but statistically nonsignificant trend was observed at 4–8 Hz (11/20 vs. 17/20;  $p =$   
 423  $0.082$ ). Also, contrast between adults and children did reveal stronger tracking in adults than  
 424 in children in bilateral supratemporal AC at 1–4 Hz (left  $[-65 \ -16 \ 7]$ ,  $p = 0.0013$ ; right  $[64 \ -$   
 425  $5 \ 6]$ ,  $p = 0.0041$ ) and 4–8 Hz (left  $[-65 \ -15 \ 9]$ ,  $p < 0.0001$ ; right  $[64 \ -8 \ 5]$ ,  $p < 0.0001$ ), but  
 426 not at  $< 1$  Hz.

427 Correlation between  $Coh_{att}$  values and children's age was statistically significant in the  
 428 right STS at  $< 1$  Hz ( $r = 0.47$ ,  $p = 0.039$ ), and in the right supratemporal AC at 4–8 Hz ( $r =$

429 0.50,  $p = 0.025$ ) (Fig. 5). No other correlations between  $Coh_{att}$  values and children' age  
 430 reached statistical significance ( $ps > 0.3$ ).

431

432 ---Place Figure 2 around here---

433 ---Place Figure 3 around here---

434 ---Place Figure 4 around Here---

435 ---Place Figure 5 around here---

436 ---Place Table 1 around Here---

437

438

#### 439 ***Cortical tracking of speech in SiN conditions***

440 In adults, group-level  $Coh_{att}$  and  $Coh_{global}$  maps at  $< 1$  Hz displayed statistically  
 441 significant ( $ps < 0.05$ ) local maxima at bilateral STS at every SNR, in the left inferior frontal  
 442 gyrus (IFG) at  $0$  dB and in the left temporal pole at  $-5$  dB.  $Coh_{bckgr}$  was not statistically  
 443 significant in any condition. At 1–4 Hz and 4–8 Hz,  $Coh_{att}$  and  $Coh_{global}$  maps displayed  
 444 statistically significant ( $ps < 0.05$ ) local maxima in AC bilaterally in every condition (Fig.4).  
 445  $Coh_{bckgr}$  was statistically significant at  $0$  dB and  $-5$  dB in right AC.

446 In children, group-level  $Coh_{att}$  and  $Coh_{global}$  maps at  $<1$  Hz displayed statistically  
 447 significant ( $ps < 0.05$ ) local maxima in bilateral STS at every SNR except at  $-5$  dB where  
 448 only  $Coh_{att}$  displayed significant local maxima (Fig.4). At 1–4 Hz,  $Coh_{att}$  and  $Coh_{global}$  maps  
 449 displayed statistically significant ( $ps < 0.05$ ) local maxima in AC bilaterally at  $+5$  and  $0$  dB,  
 450 and only  $Coh_{att}$  displayed significance coherence in right AC at  $-5$  dB (Fig.4). At 4–8 Hz,  
 451  $Coh_{att}$  and  $Coh_{global}$  maps displayed statistically significant ( $ps < 0.05$ ) local maxima only at  
 452 right AC at  $+5$  and  $0$  dB, but not at  $-5$  dB (Fig.4).  $Coh_{bckgr}$  was not statistically significant in  
 453 any condition and frequency band of interest.

454

455 ***Cortical processing of the auditory scene in SiN conditions***

456 In adults,  $Coh_{att}$  was stronger than  $Coh_{global}$ , i.e., MEG signals tracked more the *Attended*  
 457 *stream* than the *Global scene*. At  $< 1$  Hz, cortical areas showing this effect included bilateral  
 458 STS at every SNR ( $+5$  dB,  $0$  dB and  $-5$  dB:  $p < 0.0001$ ) and left inferior frontal gyrus at  $0$  dB.  
 459 Significantly stronger  $Coh_{att}$  than  $Coh_{global}$  was found at bilateral AC at every SNR at 1–4 Hz  
 460 ( $+5$  dB,  $p = 0.0004$ ;  $0$  dB,  $p = 0.0003$ ;  $-5$  dB,  $p = 0.0001$ ) and 4–8 Hz ( $+5$  dB,  $p < 0.0001$ ;  $0$   
 461 dB,  $p < 0.0001$ ;  $-5$  dB,  $p = 0.0005$ ).

462 In children,  $Coh_{att}$  at  $< 1$  Hz was statistically significantly stronger than  $Coh_{global}$  in  
 463 bilateral STS at every SNR ( $+5$  dB,  $0$  dB and  $-5$  dB:  $ps < 0.0001$ ) and in central opercular  
 464 cortex at  $-5$  dB. At 1–4 Hz, significantly stronger  $Coh_{att}$  than  $Coh_{global}$  was found in right STS  
 465 ( $+5$  dB,  $p = 0.0011$ ;  $0$  dB,  $p = 0.0011$ ;  $-5$  dB,  $p = 0.0042$ ). At 4–8 Hz, significantly stronger  
 466  $Coh_{att}$  than  $Coh_{global}$  was found at  $-5$  dB and in a non-auditory area (left superior frontal  
 467 gyrus;  $p = 0.034$ ).

468

469 ***Comparison of the tracking in adults vs. children***

470 The comparison of coherence values between adults and children revealed that tracking  
 471 at frequencies  $< 1$  Hz was stronger in adults than children in left inferior frontal gyrus at  $0$  dB  
 472 ( $p = 0.030$ ) and in bilateral STS at  $-5$  dB (left,  $p = 0.0003$ ; right,  $p = 0.0056$ ). At 1–4 Hz,  
 473  $Coh_{att}$  was significantly higher in adults than in children in bilateral AC at every SNR ( $ps <$   
 474  $0.05$ ) except at  $0$  dB in the right AC where this effect was only marginally significant ( $p =$   
 475  $0.054$ ). At 4–8 Hz,  $Coh_{att}$  was significantly higher in adults than in children in bilateral AC at  
 476 every SNR ( $ps < 0.0001$ ) (Fig. 6).

477 In contrast, no brain area displayed significantly stronger  $Coh_{att}$  in children than in  
 478 adults at any frequency band of interest.

--Place Figure 6 around here--

### ***Effect of age group, SNR, and hemispheric lateralization on cortical tracking of speech***

The effect of age group, SNR, and hemispheric lateralization on cortical tracking of speech was sought for with 3-way repeated measures ANOVA for the three frequency bands of interest separately. Since both adults and children's brains track preferentially the *Attended stream* rather than the *Global scene*, the ANOVA was performed on  $Coh_{att}$  values only.

At  $< 1$  Hz, the ANOVA revealed a significant main effect of noise level on  $Coh_{att}$  ( $F_{3,114} = 66.64, p < 0.0001$ ), a significant interaction between SNR condition and age group ( $F_{3,114} = 4.23, p = 0.0071$ ), and a significant interaction between SNR condition and hemispheric lateralization ( $F_{3,114} = 9.35, p < 0.0001$ ), but no other significant effects ( $ps > 0.05$ ). In particular, there was no significant interaction between age group and hemispheric lateralization ( $F_{1,38} = 0.07, p = 0.79$ ), showing that the effect of noise on hemispheric lateralization was similar in both age groups.

Figure 7 illustrates these effects identified on cortical tracking of *Attended speech* stream. The main effect of noise was explained by a decrease in  $Coh_{att}$  as SNR increased. The interaction between SNR condition and age group was explained by a faster decrease in children's than adults'  $Coh_{att}$  as a function of decreasing SNR (see Figs. 4 and 7). Supporting this interpretation, adults had higher  $Coh_{att}$  than children at  $-5$  dB ( $t_{38} = 3.88, p = 0.0004$ ;  $t$ -test) but not at  $0$ ,  $+5$  dB and *Noiseless* ( $ps > 0.17$ ). The interaction between SNR condition and hemispheric lateralization was explained by a faster decrease in  $Coh_{att}$  in the right than the left STS as a function of decreasing SNR (see Figs. 4 and 6). Supporting this interpretation, post-hoc comparisons revealed that  $Coh_{att}$  at right STS decreased as soon as the

504 *Multitalker background* was added (*Noiseless* vs.  $+5$  dB:  $t_{19} = 4.9$ ,  $p < 0.0001$ ) and it further  
 505 diminished as SNR decreased ( $+5$  dB vs.  $0$  dB,  $t_{19} = 4.1$ ,  $p = 0.0002$ ;  $0$  dB vs.  $-5$  dB,  $t_{19} =$   
 506  $4.23$ ,  $p = 0.0001$ ). In contrast,  $Coh_{att}$  in the left STS decreased significantly only in the two  
 507 noisiest conditions (*Noiseless* vs.  $+5$  dB,  $t_{19} = 0.49$ ,  $p = 0.62$ ;  $+5$  dB vs.  $0$  dB,  $t_{19} = 3.11$ ,  $p =$   
 508  $0.0035$ ;  $0$  dB vs.  $-5$  dB,  $t_{19} = 5.3$ ,  $p < 0.0001$ ).

509 At 1–4 Hz, the ANOVA revealed a significant main effect of age group on  $Coh_{att}$  ( $F_{3,114}$   
 510  $= 10.04$ ,  $p = 0.003$ ), a significant main effect of hemispheric lateralization ( $F_{3,114} = 10.04$ ,  $p =$   
 511  $0.003$ ), no significant main effect of the SNR condition ( $F_{3,114} = 1.53$ ,  $p = 0.21$ ), and no  
 512 significant interactions ( $ps > 0.05$ ). The main effect of age group was due to higher  $Coh_{att}$  in  
 513 adults than in children. The main effect of hemispheric lateralization was explained by higher  
 514  $Coh_{att}$  values in the right than the left AC.

515 At 4–8 Hz, the ANOVA revealed a significant main effect of age group on  $Coh_{att}$  ( $F_{3,114}$   
 516  $= 54.64$ ,  $p < 0.0001$ ), a significant main effect of noise level ( $F_{3,114} = 13.96$ ,  $p < 0.0001$ ), a  
 517 significant effect of hemispheric lateralization ( $F_{3,114} = 7.37$ ,  $p = 0.0099$ ), a significant  
 518 interaction between SNR condition and age group ( $F_{3,114} = 10.08$ ,  $p < 0.0001$ ), and no other  
 519 significant interactions ( $ps > 0.05$ ). The main effect of age group was explained by higher  
 520  $Coh_{att}$  in adults than in children at all SNRs ( $ps < 0.001$ ). The interaction between SNR  
 521 condition and age group was explained by the presence of SNR-related modulation in adults’  
 522  $Coh_{att}$  and the absence of such modulation in children’s  $Coh_{att}$  (see Fig. 7). Indeed, adults’  
 523  $Coh_{att}$  (mean across hemispheres) was significantly higher at intermediate SNRs ( $5$  dB and  $0$   
 524 dB) than in *Noiseless* ( $5$  dB,  $t_{19} = 4.29$ ,  $p = 0.0004$ ;  $0$  dB,  $t_{19} = 2.85$ ,  $p = 0.010$ ) and at  $-5$  dB ( $5$   
 525 dB,  $t_{19} = 5.26$ ,  $p < 0.0001$ ;  $0$  dB,  $t_{19} = 5.20$ ,  $p < 0.0001$ ), significantly higher at  $5$  dB than at  $0$   
 526 dB ( $t_{19} = 2.30$ ,  $p = 0.033$ ), and marginally higher in *Noiseless* than at  $-5$  dB ( $t_{19} = 1.96$ ,  $p =$   
 527  $0.065$ ). The main effect of hemispheric lateralization was explained by higher or marginally



528 higher  $Coh_{att}$  in right than left AC in every SNR condition (*noiseless*,  $t_{39} = 2.06$ ,  $p = 0.046$ ; 5  
 529 *dB*,  $t_{39} = 2.37$ ,  $p = 0.023$ ; *0 dB*,  $t_{39} = 1.93$ ,  $p = 0.061$ ; *-5 dB*,  $t_{39} = 1.71$ ,  $p = 0.095$ ).

530

531 ---Place Figure 7 around Here ---

## 532 Discussion

533 This study discloses commonalities between children and adult's cortical tracking of  
 534 SiN. First, both children and adults' auditory systems similarly tracked the attended speaker's  
 535 voice more than the global auditory scene at  $< 1$  Hz and 1–4 Hz. Second, cortical tracking of  
 536 the attended stream in SiN conditions was at  $< 1$  Hz similarly left-hemisphere-dominant in  
 537 children and adults. Furthermore, in both groups, the STS was the main brain area  
 538 underpinning this tracking at  $< 1$  Hz. Compared with adults, children displayed (i) reduced  
 539 cortical tracking of speech at 1–4 Hz, and particularly at 4–8 Hz (even in noiseless  
 540 conditions); (ii) increasing multitalker background level compromised children more than  
 541 adults in cortical tracking of speech at  $< 1$  Hz, and (iii) children did not exhibit selective  
 542 cortical representation of SiN at 4–8 Hz.

543

### 544 *Inaccurate cortical tracking of speech at 4–8 Hz in children*

545 Studies previously reported that ongoing cortical oscillations track speech regularities,  
 546 especially at syllable timescale, which corresponds to 4–8 Hz frequencies (Ding and Simon,  
 547 2012b; Gross et al., 2013; Koskinen and Seppä, 2014; Ding et al., 2016). Since the strength of  
 548 this 4–8 Hz cortical tracking is related to speech intelligibility (Luo and Poeppel, 2007; Peelle  
 549 et al., 2013; Doelling et al., 2014), it has been hypothesized to reflect active speech perception  
 550 mechanisms, very likely involved in parsing incoming connected speech into discrete syllabic  
 551 units (Giraud and Poeppel, 2012; Teng et al., 2017).



552 We demonstrated that children's auditory system is less proficient than adults' auditory  
 553 system at tracking the attended speech envelope at 1–4 Hz and 4–8 Hz. Still, without noise,  
 554 about half of children showed significant cortical tracking of the attended speech envelope at  
 555 1–4 Hz and 4–8 Hz. Crucially, cortical tracking of speech envelope at syllable rate correlated  
 556 in the right AC positively with the children's age.

557 Furthermore, 4–8 Hz tracking was sensitive to noise intensity so that the number of  
 558 children with significant tracking decreased with increasing noise level from 11 subjects in  
 559 *Noiseless* to only 2 at  $-5$  dB. Finally, at 4–8 Hz, children did not exhibit the selective tracking  
 560 of speech in auditory areas seen in adults.

561 These results are at odds with at least one of the views claiming that 1) the sensitivity to  
 562 syllables is acquired early in age and that 2) tracking at 4–8 Hz relates to processing of  
 563 syllabic units. Several studies highlighted the early-developed ability of infants and children  
 564 to discriminate syllables. Neurophysiological evidence of syllable discrimination has been  
 565 found already in preterm infants (Mahmoudzadeh et al., 2013) and 8-month-old infants are  
 566 able to segregate newly learned words from syllable strings (Saffran et al., 1996).  
 567 Furthermore, speech slow amplitude modulations are one of the first cues that children  
 568 identify when they listen to speech (Nitttrouer, 2006), allowing them to detect syllable  
 569 boundaries, which is mandatory for an accurate perception of speech (Goswami, 2011;  
 570 Poelmans et al., 2011). However, recent findings indicate that children under 10 years are less  
 571 accurate than adults at identifying syllable boundaries when these are only defined by  
 572 amplitude modulations in temporal envelope (Cameron et al., 2018), and that theta band  
 573 cortical tracking is not speech-specific (Molinaro and Lizarazu, 2017). Also questioning the  
 574 link between syllable processing and the 4–8-Hz tracking is the consistent finding that such  
 575 coupling is right-hemisphere dominant (Luo and Poeppel, 2007; Giraud and Poeppel, 2012;  
 576 Gross et al., 2013; Peelle et al., 2013). In this context, our results argue for progressive

577 evolution from childhood to adulthood of abilities to track the acoustic envelope of speech at  
 578 4–8 Hz.

579

#### 580 ***Noise easily corrupts cortical tracking of speech in children***

581 In adverse listening conditions (i.e.,  $-5$  dB), auditory system lost, in a substantial  
 582 proportion of children (70%), the capability to track the *Attended stream* at  $< 1$  Hz whereas  
 583 80% of adults exhibited significant tracking in this condition. Since children's SiN  
 584 behavioural performances are typically lower than those of adults (Elliott, 1979), we can  
 585 postulate that the poor performance was at least partially related to a limited central auditory  
 586 capacity to segregate the *Attended stream* from the *Multitalker background* at  $< 1$  Hz when  
 587 SNR decreased. This ability of the auditory system likely improves during adolescence, given  
 588 the outcome in young adults reported here and elsewhere (Ding and Simon, 2012a, 2013b;  
 589 Vander Ghinst et al., 2016). Hence, our study argues for a developmental origin of the  
 590 selective cortical tracking of the *Attended stream* at  $< 1$  Hz. These data are in line with our  
 591 results and previous psychoacoustic studies that demonstrated children's poor speech  
 592 comprehension in adverse listening conditions (Johnson, 2000; Talarico et al., 2007; Neuman  
 593 et al., 2010; Klatte et al., 2013).

594

#### 595 ***Children's and adults' auditory system tracks the attended speech stream in SiN conditions*** 596 ***at $< 1$ Hz and at 1–4 Hz.***

597 At  $< 1$  Hz and 1–4 Hz, coupling between envelopes of the listened sounds and the  
 598 activity of non-primary auditory cortex was stronger with the *Attended stream* than with the  
 599 *Global scene*, both in children and adults. This finding is in line with former studies  
 600 performed in adults (Ding and Simon, 2012a; Mesgarani and Chang, 2012; Ding and Simon,  
 601 2013b; Zion Golumbic et al., 2013; Vander Ghinst et al., 2016). Yet, and in contradiction with

our initial hypothesis, the current study is the first to demonstrate that this selective tracking already exists in children, at least up to a certain noise level. The preferential tracking of the slowest ( $< 1$  Hz) speech modulations took place, like in adults, at bilateral STS, demonstrating that this brain area extracts or has a preferential access to the *Attended stream* in reasonable SNR conditions. Still, the preferential tracking of the *Attended stream* at left IFG at  $0$  dB was higher in adults than in children. Moreover, the absence of specific tracking of the *Multitalker background* argues for an object-based neural coding of the attended speaker's voice in children's higher-order auditory cortical areas up to a certain SNR level (Simon, 2014; Puvvada and Simon, 2017). Interestingly, at 1–4 Hz, this selective tracking occurred in bilateral AC in adults but only in right AC in children. Since recent findings have shown that perceptually relevant word segmentation takes place in left temporal cortex (Keitel et al., 2018), the lack of selective cortical tracking of speech at word repetition rate (1–4 Hz) in left temporal cortex could partly explain SiN difficulties in children.

#### ***Effects of the multitalker background on hemispheric lateralization of cortical tracking of speech at $< 1$ Hz***

As demonstrated here and elsewhere (Power et al., 2012; Vander Ghinst et al., 2016; Destoky et al., 2019), the left-hemisphere cortical tracking of speech at  $< 1$  Hz is essentially preserved in a multitalker background up to a SNR of 0 dB, while it is compromised in the right hemisphere as soon as a background noise is added. Ours is the first study to demonstrate that this hemispheric asymmetry in cortical tracking occurred similarly in children and in adults, but with the noticeable difference that children lost the tracking in the more challenging conditions.

Left-hemisphere-dominant noise-resistant cortical tracking of speech at STS (and IFG in adults) could imply an active cognitive process that promotes speech recognition

(Schroeder et al., 2008; Schroeder and Lakatos, 2009; Power et al., 2012) through increased access to lexical and semantic representations (Binder et al., 2009; Liebenthal et al., 2014). This left-lateralized process is likely related to correct identification and comprehension of the targeted auditory stream (Alain et al., 2005; Bishop and Miller, 2009). Since the coupling between cortical oscillations and the low-frequency rhythmic structure of an attended acoustic stream seems to be under attentional control (Lakatos et al., 2013), the differential hemispheric effect of noise on cortical tracking of speech could be related to mechanisms of selective attention. As noise impairs children more strongly than adults in addition to auditory- and speech-related tasks also in non-auditory cognitive processes, such as reading and writing (for a review, see Klatte et al., 2013), we can hypothesize that the detrimental effect of acute and chronic noise exposure on different cognitive functions is at least partially related to the crucial attentional load needed to understand speech in adverse hearing environment.

## Conclusion

The ability of children's brains to track speech temporal envelopes at syllable rate (4–8 Hz) was drastically reduced in comparison with adults regardless of the SNR. Similarly as adults, children displayed stronger tracking of the *Attended stream* than of the *Global scene* in SiN conditions at phrasal and word rates, but their tracking ability was more easily corrupted by increasing noise. Children's poor SiN comprehension performances were therefore likely related to a limited central auditory capacity to segregate the *Attended stream* from the *Multitalker background* at phrasal and word rates as a function of decreasing SNR and at 4–8 Hz regardless of the SNR. These results further elucidate the neurophysiological mechanisms accounting for children's difficulties to adequately segregate speech in informational masking conditions.

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654 **References**

655

656 Alain C, Reinke K, McDonald KL, Chau W, Tam F, Pacurar A, Graham S (2005) Left  
657 thalamo-cortical network implicated in successful speech separation and identification.  
658 *NeuroImage* 26:592-599.

659 Ashburner J, Friston KJ (1999) Nonlinear spatial normalization using basis functions. *Hum*  
660 *Brain Mapp* 7:254-266.

661 Ashburner J, Neelin P, Collins DL, Evans A, Friston K (1997) Incorporating prior knowledge  
662 into image registration. *NeuroImage* 6:344-352.

663 Berman S, Friedman D (1995) The development of selective attention as reflected by event-  
664 related brain potentials. *J Exp Child Psychol* 59:1-31.

665 Binder JR, Desai RH, Graves WW, Conant LL (2009) Where is the semantic system? A  
666 critical review and meta-analysis of 120 functional neuroimaging studies. *Cereb*  
667 *Cortex* 19: 2767-2796.

668 Bishop CW, Miller LM (2009) A multisensory cortical network for understanding speech in  
669 noise. *J Cogn Neurosci* 21:1790-1805.

670 Bortel R, Sovka P (2007) Approximation of statistical distribution of magnitude squared  
671 coherence estimated with segment overlapping. *Signal Processing* 87:1100-1117.

672 Bourguignon M, Piitulainen H, De Tiege X, Jousmäki V, Hari R (2015) Corticokinematic  
673 coherence mainly reflects movement-induced proprioceptive feedback. *NeuroImage*  
674 106:382-390.

675 Bourguignon M, Jousmäki V, Op de Beeck M, Van Bogaert P, Goldman S, De Tiege X  
676 (2012) Neuronal network coherent with hand kinematics during fast repetitive hand  
677 movements. *NeuroImage* 59:1684-1691.

- 678 Bourguignon M, De Tiege X, Op de Beeck M, Ligt N, Paquier P, Van Bogaert P, Goldman  
679 S, Hari R, Jousmäki (2013) The pace of prosodic phrasing couples the listener's cortex  
680 to the reader's voice. *Hum Brain Mapp* 34:314-326.
- 681 Bourguignon M, Molinaro N, Wens V (2017) Contrasting functional imaging parametric  
682 maps: The mislocation problem and alternative solutions. *NeuroImage* 169:200–211.
- 683 Cameron S, Chong-White N, Mealings K, Beechey T, Dillon H, Young T (2018) The parsing  
684 syllable envelopes test for assessment of amplitude modulation discrimination skills in  
685 children: development, normative data, and test-retest reliability studies. *J Am Acad*  
686 *Audiol* 29:151-163.
- 687 Carrette E, Op de Beeck M, Bourguignon M, Boon P, Vonck K, Legros B, Goldman S, Van  
688 Bogaert P, De Tiege X (2011) Recording temporal lobe epileptic activity with MEG in  
689 a light-weight magnetic shield. *Seizure* 20:414-418.
- 690 Clumeck C, Suarez Garcia S, Bourguignon M, Wens V, Op de Beeck M, Marty B, Deconinck  
691 N, Soncarrieu MV, Goldman S, Jousmäki V, Van Bogaert P, De Tiege X (2014)  
692 Preserved coupling between the reader's voice and the listener's cortical activity in  
693 autism spectrum disorders. *PloS one* 9:e92329.
- 694 Dale AM, Sereno MI (1993) Improved localizadon of cortical activity by combining EEG and  
695 MEG with MRI cortical surface reconstruction: a linear approach. *J Cogn Neurosci*  
696 5:162-176.
- 697 De Tiege X, Op de Beeck M, Funke M, Legros B, Parkkonen L, Goldman S, Van Bogaert P  
698 (2008) Recording epileptic activity with MEG in a light-weight magnetic shield.  
699 *Epilepsy Res* 82:227-231.
- 700 Demanez L, Dony-Closon B, Lhonneux-Ledoux E, Demanez JP (2003) Central auditory  
701 processing assessment: a French-speaking battery. *Acta Otorhinolaryngol Belg*  
702 57:275-290.

- 703 Destoky F, Philippe M, Bertels J, Verhasselt M, Coquelet N, Vander Ghinst M, Wens V, De  
704 Tiège X, Bourguignon M (2019) Comparing the potential of MEG and EEG to  
705 uncover brain tracking of speech temporal envelope. *NeuroImage* 184:201-213.
- 706 Ding N, Simon JZ (2012a) Emergence of neural encoding of auditory objects while listening  
707 to competing speakers. *Proc Natl Acad Sci U S A* 109:11854-11859.
- 708 Ding N, Simon JZ (2012b) Neural coding of continuous speech in auditory cortex during  
709 monaural and dichotic listening. *J Neurophysiol* 107:78-89.
- 710 Ding N, Simon JZ (2013a) Robust cortical encoding of slow temporal modulations of speech.  
711 *Adv Exp Med Biol* 787:373-381.
- 712 Ding N, Simon JZ (2013b) Adaptive temporal encoding leads to a background-insensitive  
713 cortical representation of speech. *J Neurosci* 33:5728-5735.
- 714 Ding N, Melloni L, Zhang H, Tian X, Poeppel D (2016) Cortical tracking of hierarchical  
715 linguistic structures in connected speech. *Nat Neurosci* 19:158-164.
- 716 Doelling KB, Arnal LH, Ghitza O, Poeppel D (2014) Acoustic landmarks drive delta-theta  
717 oscillations to enable speech comprehension by facilitating perceptual parsing.  
718 *NeuroImage* 85 Pt 2:761-768.
- 719 Drullman R, Festen JM, Plomp R (1994) Effect of temporal envelope smearing on speech  
720 reception. *J Acoust Soc Am* 95:1053-1064.
- 721 Elliott LL (1979) Performance of children aged 9 to 17 years on a test of speech intelligibility  
722 in noise using sentence material with controlled word predictability. *J Acoust Soc Am*  
723 66:651-653.
- 724 Faes L, Pinna GD, Porta A, Maestri R, Nollo G (2004) Surrogate data analysis for assessing  
725 the significance of the coherence function. *IEEE Trans Biomed Eng* 51:1156-1166.
- 726 Ferstl EC, Walther K, Guthke T, von Cramon DY (2005) Assessment of story comprehension  
727 deficits after brain damage. *J Clin Exp Neuropsychol* 27:367-384.



- 728 Giraud AL, Poeppel D (2012) Cortical oscillations and speech processing: emerging  
729 computational principles and operations. *Nat Neurosci* 15:511-517.
- 730 Goswami U (2011) A temporal sampling framework for developmental dyslexia. *Trends*  
731 *Cogn Sci* 15:3-10.
- 732 Gramfort A, Luessi M, Larson E, Engemann DA, Strohmeier D, Brodbeck C, Parkkonen L,  
733 Hamalainen MS (2014) MNE software for processing MEG and EEG data.  
734 *NeuroImage* 86:446-460.
- 735 Gross J, Kujala J, Hamalainen M, Timmermann L, Schnitzler A, Salmelin R (2001) Dynamic  
736 imaging of coherent sources: Studying neural interactions in the human brain. *Proc*  
737 *Natl Acad Sci U S A* 98:694-699.
- 738 Gross J, Hoogenboom N, Thut G, Schyns P, Panzeri S, Belin P, Garrod S (2013) Speech  
739 rhythms and multiplexed oscillatory sensory coding in the human brain. *PLoS Biol*  
740 11:e1001752.
- 741 Hall JW, 3rd, Buss E, Grose JH (2005) Informational masking release in children and adults.  
742 *J Acoust Soc Am* 118:1605-1613.
- 743 Halliday DM, Rosenberg JR, Amjad AM, Breeze P, Conway BA, Farmer SF (1995) A  
744 framework for the analysis of mixed time series/point process data--theory and  
745 application to the study of physiological tremor, single motor unit discharges and  
746 electromyograms. *Prog Biophys Mol Biol* 64:237-278.
- 747 Hämäläinen ML, Lin F-H, Mosher J (2010) Anatomically and functionally constrained  
748 minimum-norm estimates. In: *MEG-an introduction to methods* (Press OU, ed), pp  
749 186-215.
- 750 Hämäläinen MS, Ilmoniemi RJ (1994) Interpreting magnetic fields of the brain: minimum  
751 norm estimates. *Med. Biol. Eng. Comput.* 32:35-42.

- 752 Hoen M, Meunier F, Grataloup C-L, Pellegrino F, Grimault N, Perrin F, Perrot X, Collet L  
 753 (2007) Phonetic and lexical interferences in informational masking during speech-in-  
 754 speech comprehension. *Speech Commun* 49:905-916.
- 755 Johnson CE (2000) Children's phoneme identification in reverberation and noise. *J Speech*  
 756 *Lang Hear Res* 43:144-157.
- 757 Karns CM, Isbell E, Giuliano RJ, Neville HJ (2015) Auditory attention in childhood and  
 758 adolescence: An event-related potential study of spatial selective attention to one of  
 759 two simultaneous stories. *Dev Cogn Neurosci* 13:53-67.
- 760 Keitel A, Gross J, Kayser C (2018) Perceptually relevant speech tracking in auditory and  
 761 motor cortex reflects distinct linguistic features. *Plos Biol* 16(3):e2004473.
- 762 Klatte M, Bergstrom K, Lachmann T (2013) Does noise affect learning? A short review on  
 763 noise effects on cognitive performance in children. *Front Psychol* 4:578.
- 764 Koskinen M, Seppa M (2014) Uncovering cortical MEG responses to listened audiobook  
 765 stories. *NeuroImage* 100:263-270.
- 766 Lakatos P, Musacchia G, O'Connell MN, Falchier AY, Javitt DC, Schroeder CE (2013) The  
 767 spectrotemporal filter mechanism of auditory selective attention. *Neuron* 77:750-761.
- 768 Leibold LJ, Neff DL (2007) Effects of masker-spectral variability and masker fringes in  
 769 children and adults. *J Acoust Soc Am* 121:3666-3676.
- 770 Liebenthal E, Desai RH, Humphries C, Sabri, Desai A (2014) The functional organization of  
 771 the left STS: a large scale meta-analysis of PET and fMRI studies of healthy adults.  
 772 *Front Neurosci* 8:289.
- 773 Lilliefors HW (1967) On the Kolmogorov-Smirnov test for normality with mean and variance  
 774 unknown. *J Am Stat Assoc* 62:399-402.
- 775 Luo H, Poeppel D (2007) Phase patterns of neuronal responses reliably discriminate speech in  
 776 human auditory cortex. *Neuron* 54:1001-1010.

- 777 Mahmoudzadeh M, Dehaene-Lambertz G, Fournier M, Kongolo G, Goudjil S, Dubois J,  
 778 Grebe R, Wallois F (2013) Syllabic discrimination in premature human infants prior to  
 779 complete formation of cortical layers. *Proc Natl Acad Sci U S A* 110:4846-4851.
- 780 Massaro DW (2017) Reading aloud to children: Benefits and implications for acquiring  
 781 literacy before schooling begins. *Am J Psychol* 130:63-72.
- 782 McCoy SL, Tun PA, Cox LC, Colangelo M, Stewart RA, Wingfield A (2005) Hearing loss  
 783 and perceptual effort: downstream effects on older adults' memory for speech. *Q J Exp*  
 784 *Psychol A* 58:22-33.
- 785 Mesgarani N, Chang EF (2012) Selective cortical representation of attended speaker in multi-  
 786 talker speech perception. *Nature* 485:233-236.
- 787 Molinaro N, Lizarazu M (2017) Delta(but not theta)-band cortical entrainment involves  
 788 speech-specific processing. *Eur J Neurosci*.
- 789 Molinaro N, Lizarazu M, Lallier M, Bourguignon M, Carreiras M (2016) Out-of-synchrony  
 790 speech entrainment in developmental dyslexia. *Hum Brain Mapp* 37:2767-2783.
- 791 Moore DR, Ferguson MA, Edmondson-Jones AM, Ratib S, Riley A (2010) Nature of auditory  
 792 processing disorder in children. *Pediatrics* 126:e382-390.
- 793 Muzik O, Chugani DC, Juhasz C, Shen C, Chugani HT (2000) Statistical parametric mapping:  
 794 assessment of application in children. *NeuroImage* 12:538-549.
- 795 Neuman AC, Wroblewski M, Hajicek J, Rubinstein A (2010) Combined effects of noise and  
 796 reverberation on speech recognition performance of normal-hearing children and  
 797 adults. *Ear Hear* 31:336-344.
- 798 Nichols TE, Holmes AP (2002) Nonparametric permutation tests for functional  
 799 neuroimaging: a primer with examples. *Hum Brain Mapp* 15:1-25.
- 800 Nittrouer S (2006) Children hear the forest. *J Acoust Soc Am* 120:1799-1802.

- 801 Oldfield RC (1971) The assessment and analysis of handedness: the Edinburgh inventory.  
 802 Neuropsychologia 9:97-113.
- 803 Peelle JE, Gross J, Davis MH (2013) Phase-locked responses to speech in human auditory  
 804 cortex are enhanced during comprehension. Cereb Cortex 23:1378-1387.
- 805 Poelmans H, Luts H, Vandermosten M, Boets B, Ghesquiere P, Wouters J (2011) Reduced  
 806 sensitivity to slow-rate dynamic auditory information in children with dyslexia. Res  
 807 Dev Disabil 32:2810-2819.
- 808 Power AJ, Foxe JJ, Forde EJ, Reilly RB, Lalor EC (2012) At what time is the cocktail party?  
 809 A late locus of selective attention to natural speech. Eur J Neurosci 35:1497-1503.
- 810 Power AJ, Colling LJ, Mead N, Barnes L, Goswami U (2016) Neural encoding of the speech  
 811 envelope by children with developmental dyslexia. Brain Lang 160:1-10.
- 812 Puvvada KC, Simon JZ (2017) Cortical representations of speech in a multitalker auditory  
 813 scene. J Neurosci 37:9189-9196.
- 814 Reiss AL, Abrams MT, Singer HS, Ross JL, Denckla MB (1996) Brain development, gender  
 815 and IQ in children. A volumetric imaging study. Brain 119 (5):1763-1774.
- 816 Reuter M, Schmansky NJ, Rosas HD, Fischl B (2012) Within-subject template estimation for  
 817 unbiased longitudinal image analysis. NeuroImage 61:1402-1418.
- 818 Rosenberg JR, Amjad AM, Breeze P, Brillinger DR, Halliday DM (1989) The Fourier  
 819 approach to the identification of functional coupling between neuronal spike trains.  
 820 Prog Biophys Mol Biol. 53:1-31.
- 821 Saffran JR, Aslin RN, Newport EL (1996) Statistical learning by 8-month-old infants. Science  
 822 274:1926-1928.
- 823 Sanes DH, Woolley SM (2011) A behavioral framework to guide research on central auditory  
 824 development and plasticity. Neuron 72:912-929.

- 825 Schroeder CE, Lakatos P (2009) Low-frequency neuronal oscillations as instruments of  
826 sensory selection. *Trends Neurosci* 32:9-18.
- 827 Schroeder CE, Lakatos P, Kajikawa Y, Partan S, Puce A (2008) Neuronal oscillations and  
828 visual amplification of speech. *Trends Cogn Sci* 12:106-113.
- 829 Simon JZ (2014) The encoding of auditory objects in auditory cortex: Insights from  
830 magnetoencephalography. *Int J Psychophysiol* 95(2):184-90. .
- 831 Simpson SA, Cooke M (2005) Consonant identification in N-talker babble is a nonmonotonic  
832 function of N. *J Acoust Soc Am* 118:2775-2778.
- 833 Sussman E, Steinschneider M (2009) Attention effects on auditory scene analysis in children.  
834 *Neuropsychologia* 47:771-785.
- 835 Talarico M, Abdilla G, Aliferis M, Balazic I, Giaprakis I, Stefanakis T, Foenander K,  
836 Grayden DB, Paolini AG (2007) Effect of age and cognition on childhood speech in  
837 noise perception abilities. *Audiol Neurotol* 12:13-19.
- 838 Taulu S, Simola J (2006) Spatiotemporal signal space separation method for rejecting nearby  
839 interference in MEG measurements. *Phys Med Biol* 51:1759-1768.
- 840 Taulu S, Simola J, Kajola M (2005) Applications of the signal space separation method. *IEEE*  
841 *Trans Signal Process* 53:3359-3372.
- 842 Teng X, Tian X, Doelling K, Poeppel D (2017) Theta band oscillations reflect more than  
843 entrainment: behavioral and neural evidence demonstrates an active chunking process.  
844 *Eur J Neurosci*
- 845 Thompson EC, Woodruff Carr K, White-Schwoch T, Otto-Meyer S, Kraus N (2017)  
846 Individual differences in speech-in-noise perception parallel neural speech processing  
847 and attention in preschoolers. *Hear Res* 344:148-157.
- 848 Vander Ghinst M, Bourguignon M, Op de Beeck M, Wens V, Marty B, Hassid S, Choufani  
849 G, Jousmäki V, Hari R, Van Bogaert P, Goldman S, De Tieghe X (2016) Left superior

850 temporal gyrus is coupled to attended speech in a cocktail-party auditory scene. J  
851 Neurosci 36:1596-1606.

852 Wens V, Marty B, Mary A, Bourguignon M, Op de Beeck M, Goldman S, Van Bogaert P,  
853 Peigneux P, De Tiège X (2015) A geometric correction scheme for spatial leakage  
854 effects in MEG/EEG seed-based functional connectivity mapping. Hum. Brain Mapp.  
855 36:4604–4621.

856 Wightman FL, Kistler DJ (2005) Informational masking of speech in children: effects of  
857 ipsilateral and contralateral distracters. J Acoust Soc Am 118:3164-3176.

858 Wightman FL, Callahan MR, Lutfi RA, Kistler DJ, Oh E (2003) Children's detection of pure-  
859 tone signals: informational masking with contralateral maskers. J Acoust Soc Am  
860 113:3297-3305.

861 Zion Golumbic EM, Ding N, Bickel S, Lakatos P, Schevon CA, McKhann GM, Goodman  
862 RR, Emerson R, Mehta AD, Simon JZ, Poeppel D, Schroeder CE (2013) Mechanisms  
863 underlying selective neuronal tracking of attended speech at a "cocktail party". Neuron  
864 77:980-991.

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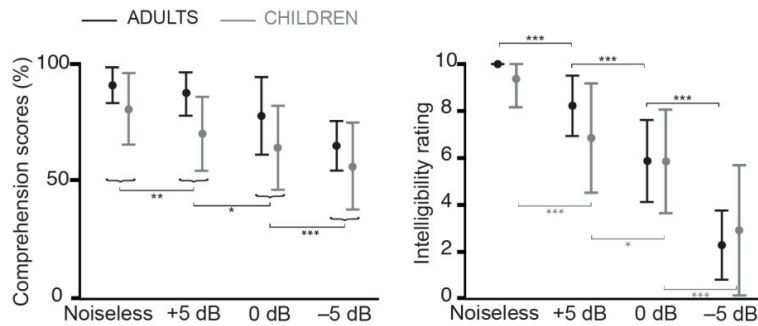
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**Figure 1:** Comprehension scores (left graph) and intelligibility ratings (right graph) in adults

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(black) and children (grey). Bars indicate the mean and range. Comprehension scores are

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reported in percentage of questions (16 for adults and 8 for children) answered correctly, and

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intelligibility ratings ranged from 0 (totally unintelligible) to 10 (perfectly intelligible). The

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comprehension and intelligibility of the Attended stream decreased significantly as SNR

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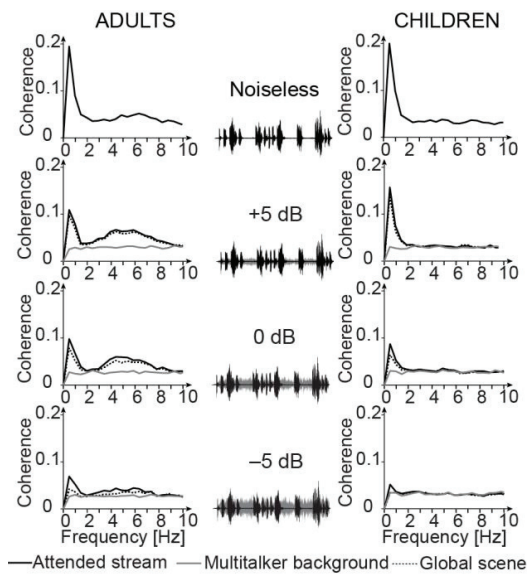
decreased. Horizontal brackets indicate the outcome of post-hoc paired *t*-tests between

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adjacent conditions (\*\* $p < 0.001$ , \*\* $p < 0.01$ , \* $p < 0.05$ ).

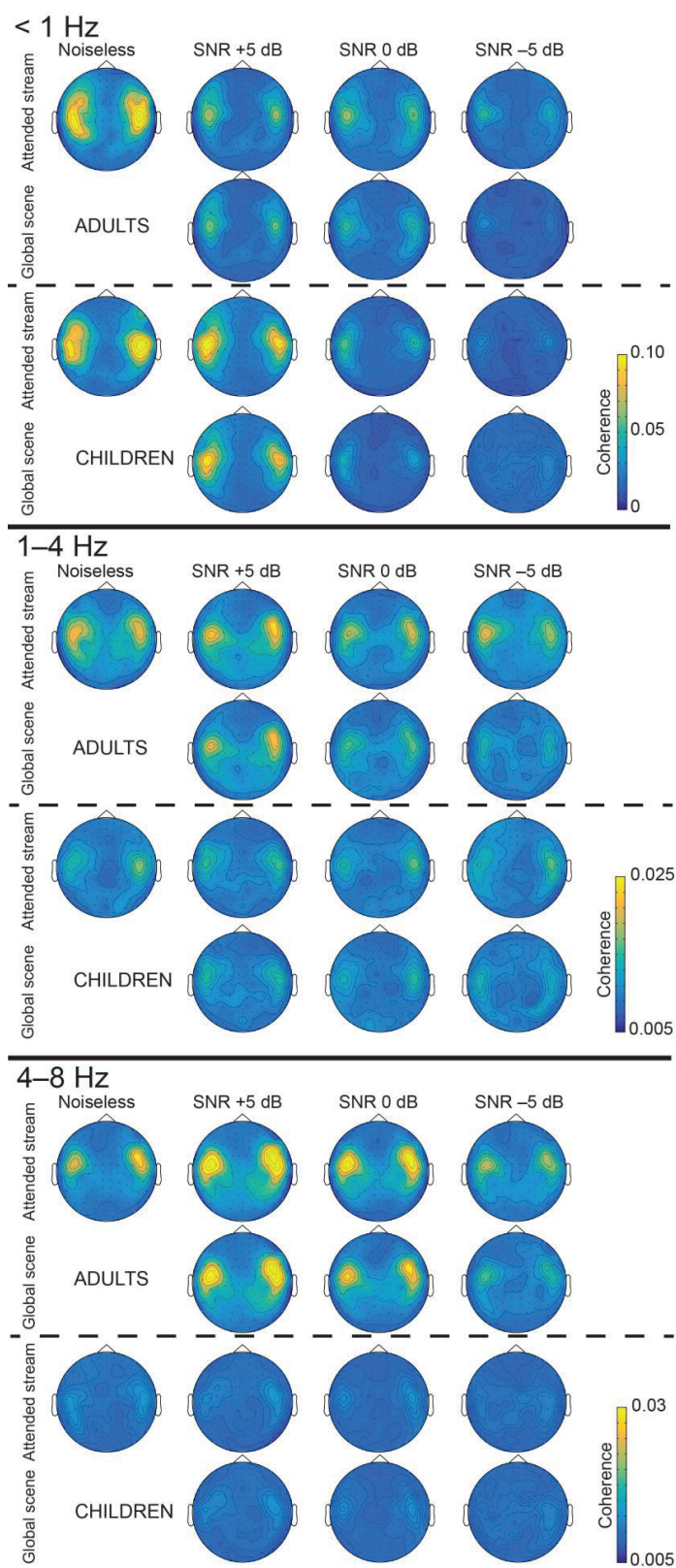
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**Figure 2:** Spectra of cortical tracking of speech in the 4 speech-in-noise conditions and corresponding sound excerpts. Group-averaged coherence spectra are shown separately for adults (left column) and children (right column), and when estimated with the temporal envelope of the different components of the auditory scene: the *Attended stream* (black connected trace), the *Multitalker background* (gray connected trace), and the *Global scene* (gray dotted trace). Each spectrum represents the mean across subjects (12 in each age group) of the maximum coherence across all sensors. The sound excerpts showcase the *Attended stream* (black traces) and the *Multitalker background* (gray traces) and their relative amplitude depending on the signal to noise ratio.





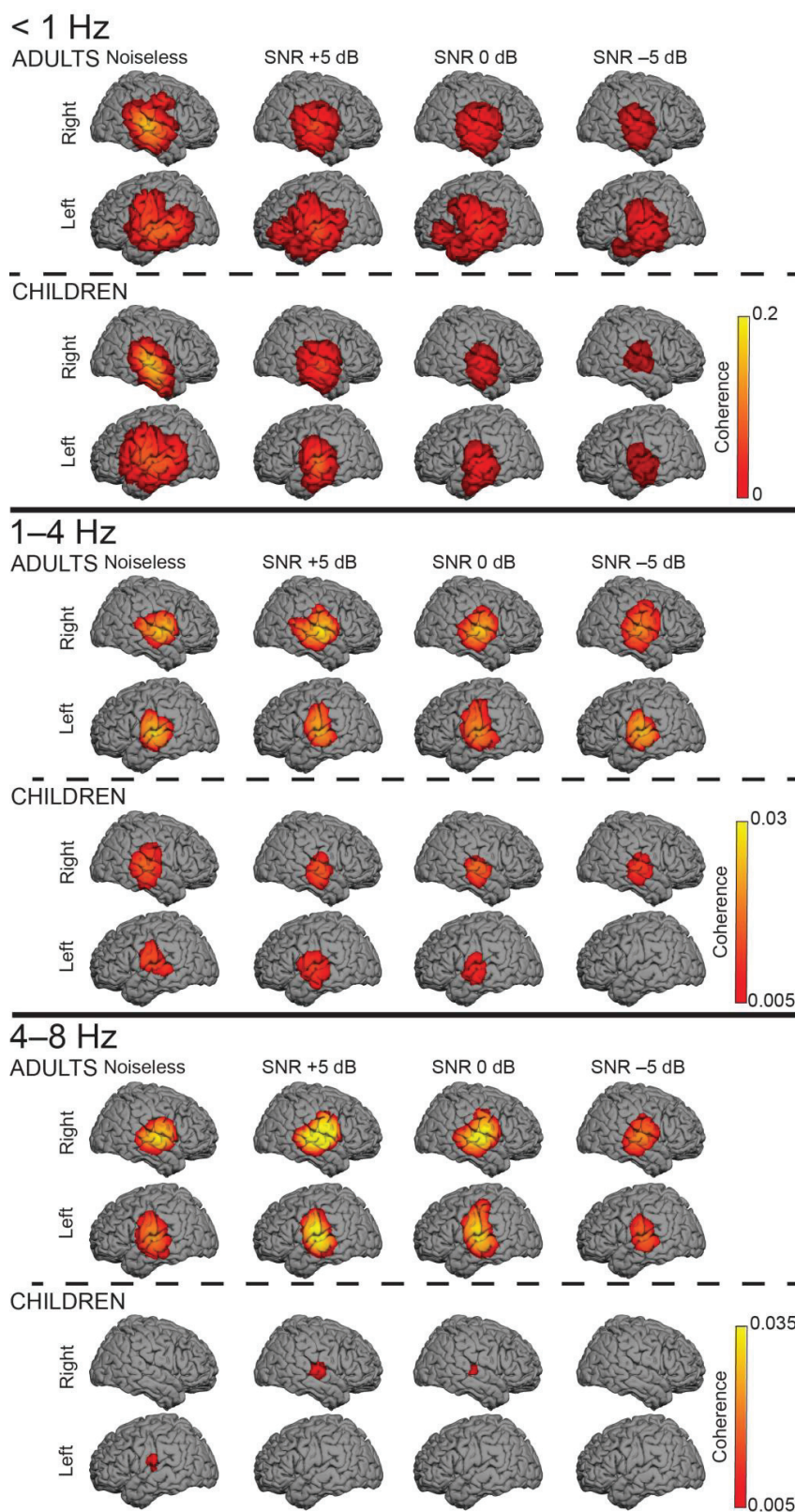
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901 **Figure 3:** Cortical tracking of speech in the sensor-space. Plots display the group-averaged  
902 coherence distributions obtained based on gradiometer data, implying that maximum  
903 coherence should peak right above generating brain sources. There is one distribution map for  
904 each frequency band of interest ( $< 1$  Hz, 1–4 Hz, 4–8 Hz), age group (adults, children)  
905 component of the auditory scene (*Attended stream*, *Global scene*), and SNR condition  
906 (*Noiseless*,  $+5$  dB,  $0$  dB,  $-5$  dB).

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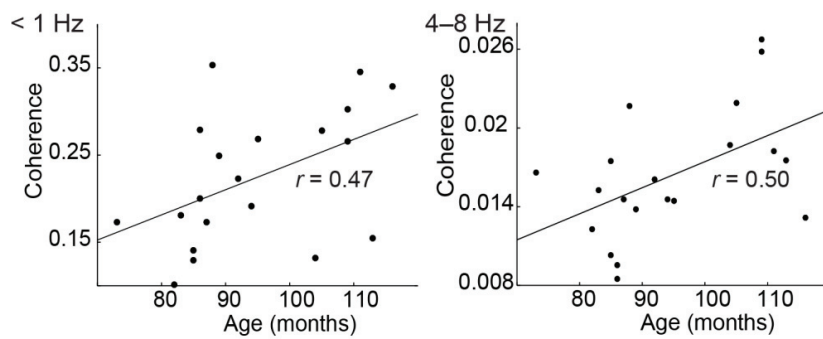
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910 **Figure 4:** Cortical tracking of the attended speech stream at < 1 Hz, 1–4 Hz, and 4–8 Hz. The  
911 group-level coherence maps ( $n = 20$  in each map) were masked statistically above the  
912 significance level (non-parametric permutation statistics). One source distribution is displayed  
913 for each possible combination of age group (adults, top panel; children, bottom panel) and  
914 SNR condition (from left to right, Noiseless, +5 dB, 0 dB, and –5 dB).

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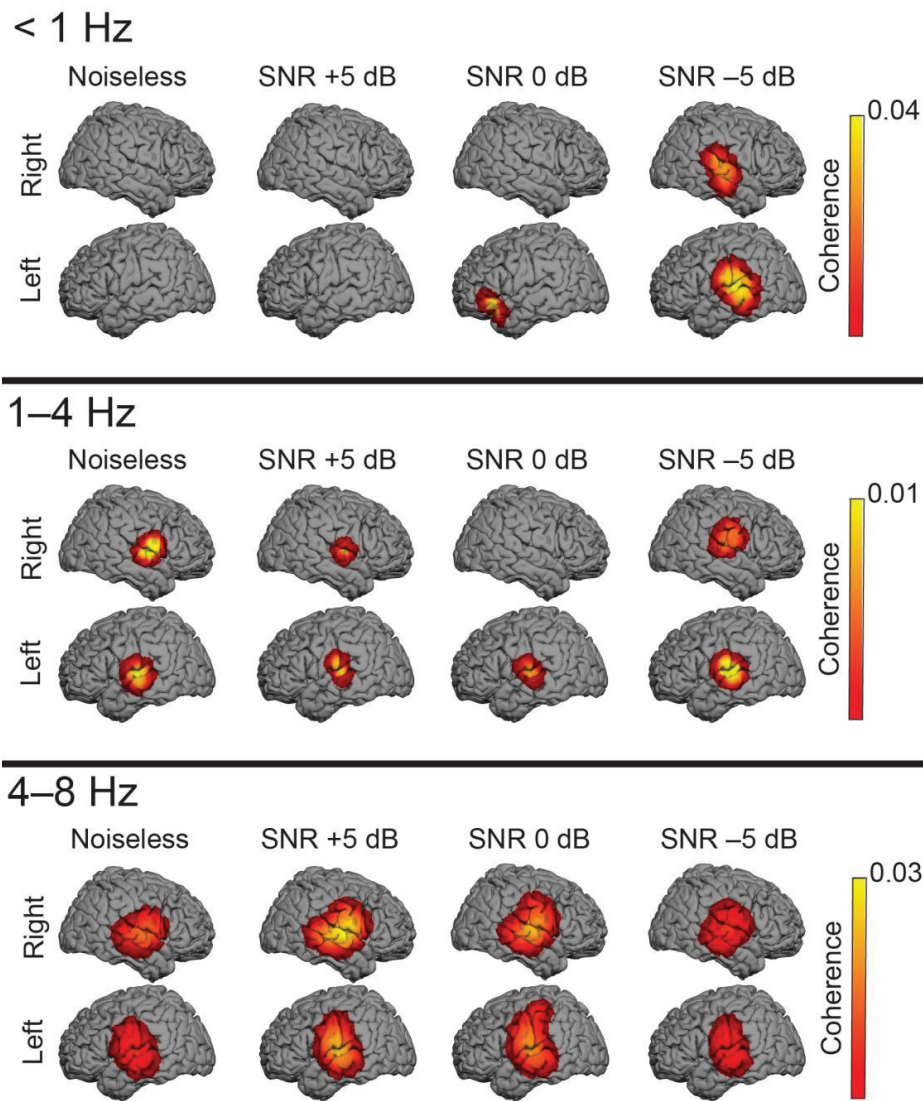
920 **Figure 5:** Correlation between children's age and their speech tracking values, depicted by

921 the peak group-level coherence, in the noiseless condition at the right superior temporal

922 sulcus at < 1 Hz and supratemporal auditory cortex at 4–8 Hz.

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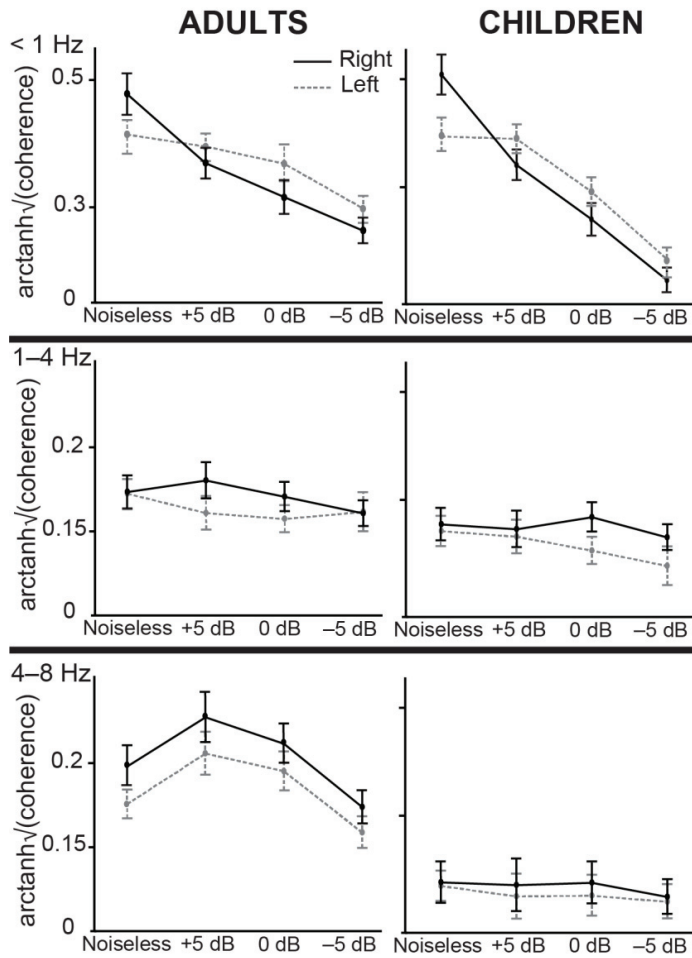


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927 **Figure 6:** Contrasts between cortical tracking of the attended speech ( $Coh_{att}$ ) in adults versus  
928 children ( $Coh_{att,adults} - Coh_{att,children}$ ) at  $< 1$  Hz, 1–4 Hz, and 4–8 Hz in all SNR conditions  
929 (Noiseless, +5 dB, 0 dB, and -5 dB). The group-level difference coherence maps ( $n = 20$  in  
930 each map) were masked statistically above the significance level.

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937 **Figure 7:** Illustration of the interaction effects identified on speech brain tracking of the  
 938 attend speech stream in adults (left column) and children (right column), at < 1 Hz, 1–4 Hz  
 939 and 4–8 Hz. Bars indicate the mean and standard error on the mean of  $f$ -transformed (with  
 940  $f(\cdot) = \text{arctanh}(\sqrt{\cdot})$ ) coherence values at the right (solid lines) and left (dashed lines) cortical  
 941 area of peak group-level coherence (superior temporal sulcus at <1 Hz, and supratemporal  
 942 auditory cortex at 1–4 Hz and 4–8 Hz).

943

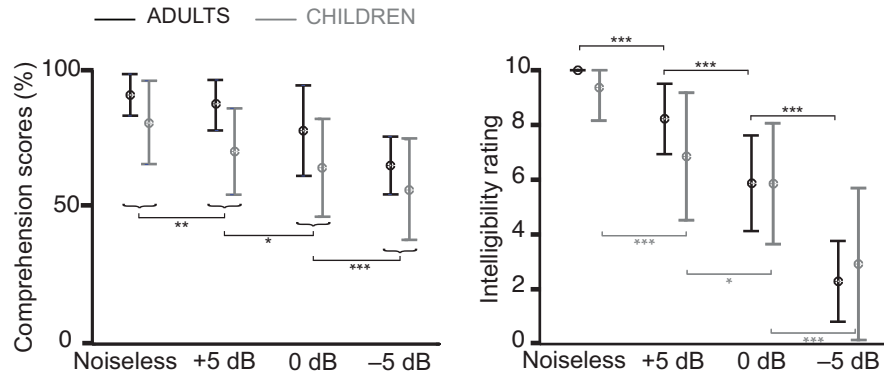
Condition	Attended stream		Multitalker background		Global scene	
	Adult	Children	Adult	Children	Adult	Children
<1 Hz						
Noiseless	20	20				
+5 dB	20	19	2	1	20	19
0 dB	20	17	1	1	18	14
-5 dB	16	6	0	4	9	1
1-4 Hz						
Noiseless	17	10				
+5 dB	16	8	2	1	14	9
0 dB	16	8	0	3	13	8
-5 dB	10	7	3	1	7	6
4-8 Hz						
Noiseless	17	11				
+5 dB	20	7	3	3	20	7
0 dB	19	5	3	4	19	5
-5 dB	15	2	7	1	13	3

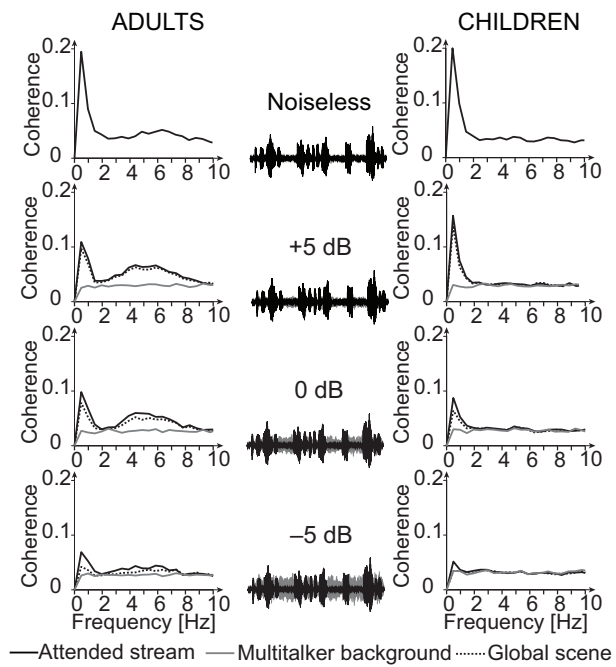
944

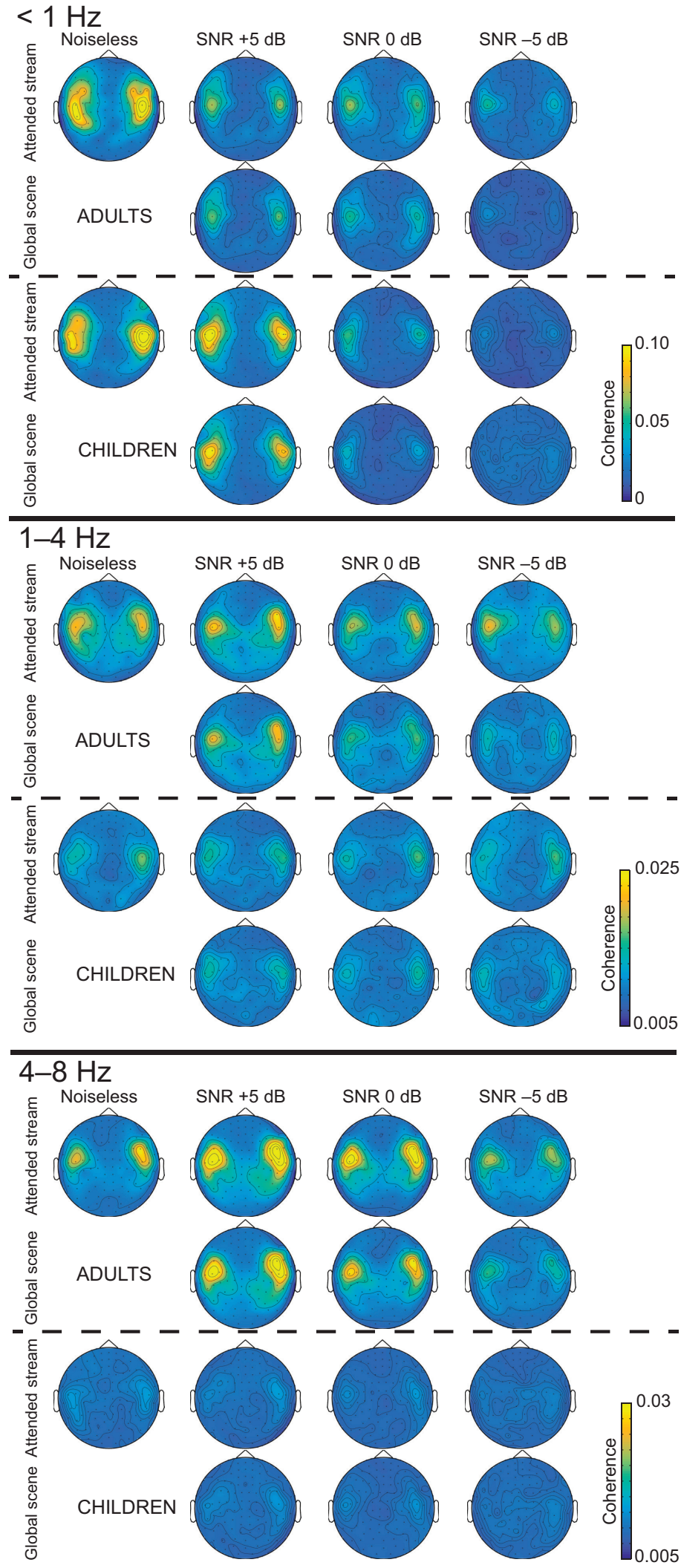
945

946 **Table 1:** Number of adults and children showing statistically significant coherence  
947 (surrogate-data-based statistics) in at least one sensor for each audio signal, condition, and  
948 frequency band of interest.









< 1 Hz

ADULTS Noiseless

SNR +5 dB

SNR 0 dB

SNR -5 dB

Right

Left

CHILDREN

Right

Left



1-4 Hz

ADULTS Noiseless

SNR +5 dB

SNR 0 dB

SNR -5 dB

Right

Left

CHILDREN

Right

Left



4-8 Hz

ADULTS Noiseless

SNR +5 dB

SNR 0 dB

SNR -5 dB

Right

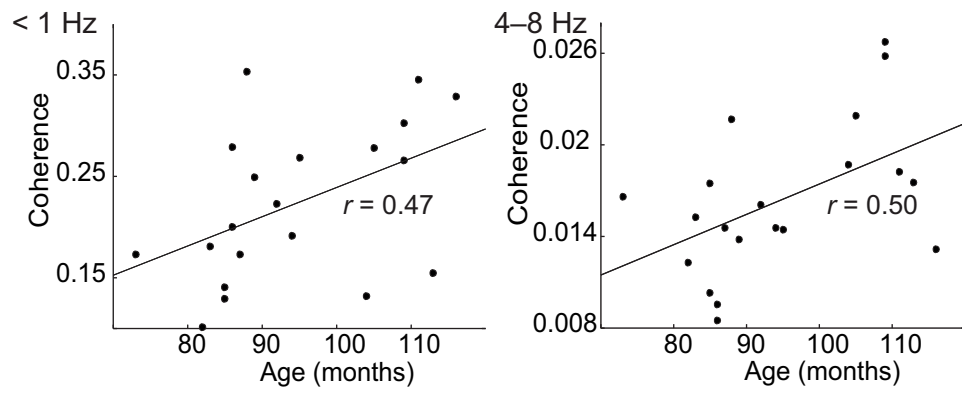
Left

CHILDREN

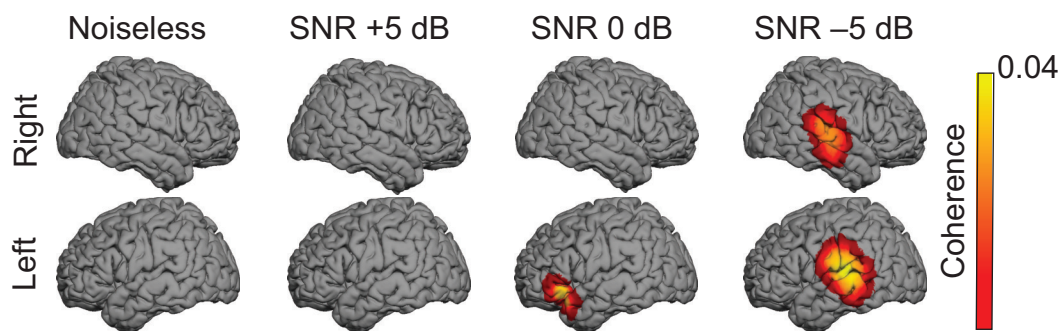
Right

Left

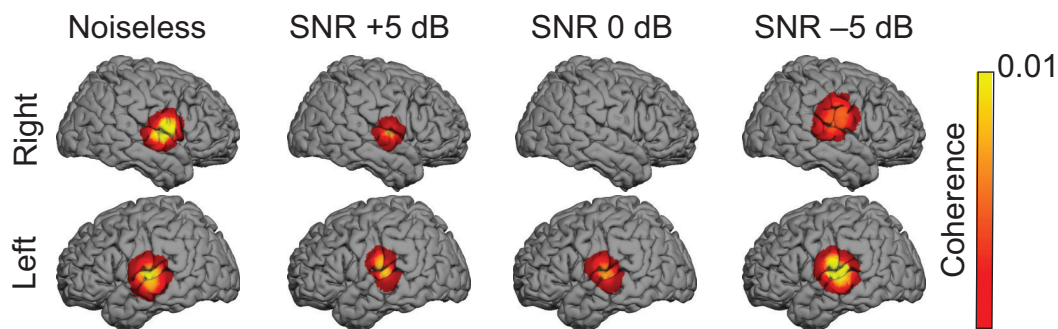




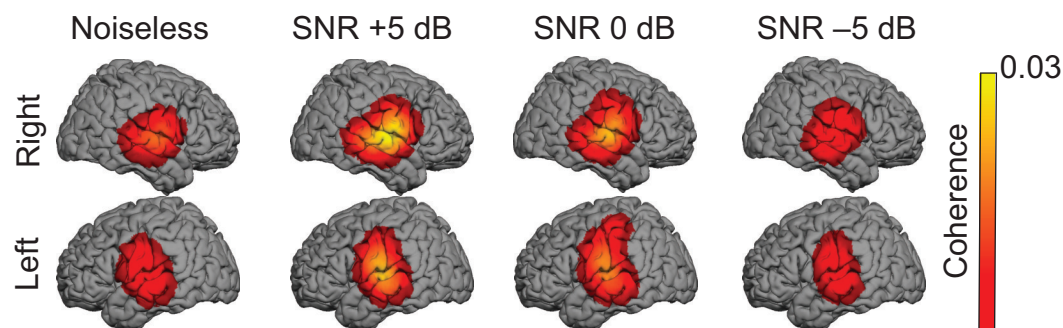
< 1 Hz



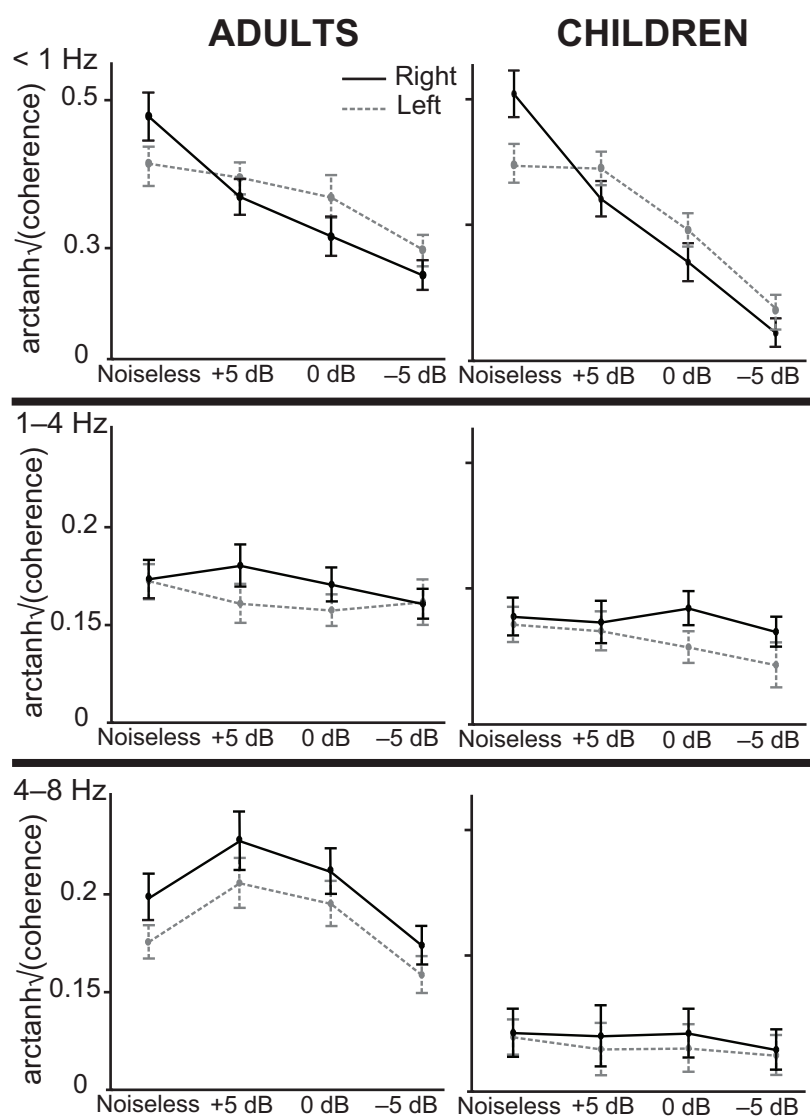
1–4 Hz



4–8 Hz







Condition	<i>Attended stream</i>		<i>Multitalker background</i>		<i>Global scene</i>	
	Adult	Children	Adult	Children	Adult	Children
<i>Noiseless</i>  <i>+5 dB</i>  <i>0 dB</i>  <i>−5 dB</i>	<1 Hz					
	20	20				
	20	19	2	1	20	19
	20	17	1	1	18	14
	16	6	0	4	9	1
	1–4 Hz					
	17	10				
	16	8	2	1	14	9
	16	8	0	3	13	8
	10	7	3	1	7	6
<i>Noiseless</i>  <i>+5 dB</i>  <i>0 dB</i>  <i>−5 dB</i>	4–8 Hz					
	17	11				
	20	7	3	3	20	7
	19	5	3	4	19	5
	15	2	7	1	13	3